


# New Proline, Alanine, Serine Repeat Sequence for Pharmacokinetic Enhancement of Anti-VEGF Single-Domain Antibody

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## ABSTRACT

Therapeutic fragmented antibodies show a poor pharmacokinetic profile that leads to frequent high-dose administration. In the current study, for the first time, a novel proline, alanine, serine (PAS) repeat sequence called PAS#208 was designed to extend the plasma half-life of a nanosized anti-vascular endothelial growth factor-A single-domain antibody. Polyacrylamide gel electrophoresis, circular dichroism, dynamic light scattering, and electrophoretic light scattering were used to assess the physicochemical properties of the newly designed PAS sequence. The effect of PAS#208 on the biologic activity of a single-domain antibody was studied using an in vitro proliferation assay. The pharmacokinetic parameters, including terminal half-life, the volume of distribution, elimination rate constant, and clearance, were determined in mice model and compared with the native protein and PAS#1(200) sequence. The novel PAS repeat sequence showed comparable physicochemical, biologic, and pharmacokinetic features to the previously reported PAS#1(200) sequence. The PAS#208 increased the hydrodynamic radius and decreased significantly the electrophoretic mobility of the

native protein without any change in zeta potential. Surprisingly, the fusion of PAS#208 to the single-domain antibody increased the binding potency. In addition, it did not alter the biologic activity and did not show any cytotoxicity on the normal cells. The PAS#208 sequence improved the terminal half-life (14-fold) as well as other pharmacokinetic parameters significantly. The simplicity as well as superior effects on half-life extension make PAS#208 sequence a novel sequence for in vivo pharmacokinetic enhancement of therapeutic fragmented antibodies.

## SIGNIFICANCE STATEMENT

In the current study, a new proline, alanine, serine (PAS) sequence was developed that showed comparable physicochemical, biological, and pharmacokinetic features to the previously reported PAS#1(200) sequence. The simplicity as well as superior effects on half-life extension make PAS#208 sequence a novel sequence for in vivo pharmacokinetic enhancement of recombinant small proteins.

## Introduction

Despite extensive researches in the field of cancer diagnosis and therapy, cancer remains one of the prominent causes of death in the world (Siegel et al., 2019). Angiogenesis is the most important and essential process in cancer development that leads to growth, metastasis, and invasion. It refers to the formation of new blood vessels from the existing vasculature. Angiogenesis inhibition interrupts the bloodstream to the

tumor and causes oxygen and nutrient deficiencies in the tumor tissues (Lin et al., 2016). Vascular endothelial growth factor (VEGF) is a key regulator of angiogenesis process, which is expressed in the most solid tumors. Many investigations have been focused on blocking of the VEGF/VEGFR2-signaling pathway that leads to the development of potent anticancer drugs. The most successful approved biopharmaceuticals for this purpose are anti-VEGF/VEGFR monoclonal antibodies (Zirlik and Duyster, 2018). Monoclonal antibodies and their fragments have now remarkably altered the outcome of cancer treatment in the clinic (Ecker et al., 2015). Although the conventional monoclonal antibodies have several clinical advantages, they suffer from immune system

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**ABBREVIATIONS:** AUC, area under the curve; CL, clearance; HEK293, human embryonic kidney 293; HRP, horseradish peroxidase; MDA-MB-231, M.D. Anderson–metastasis breast-cancer; Nb, nanobody; PAS, proline, alanine, serine; PEG, polyethylene glycol; rhVEGF<sub>A165</sub>, recombinant human VEGF<sub>A165</sub>; RT, room temperature; T<sub>1/2</sub>, terminal half-life; VEGF, vascular endothelial growth factor; VEGFR, VEGF receptor; V<sub>d</sub>, volume of distribution.

stimulation and low accessibility to the hidden antigens in the solid tumors (Muyldermans, 2013; Mendler et al., 2016). Recently, there is great attention to next-generation antibodies. Single-domain antibodies, also known as nanobodies, are antibody fragments derived from Camelidae heavy-chain antibodies. Single-domain antibodies are the smallest antigen-binding fragments that provide many advantages in comparison with the commercially available antibodies, such as small size, low immunogenicity, high affinity, high solubility, high stability, high expression in the prokaryotic systems, and easy manipulation (Iezzi et al., 2018). Moreover, they can easily penetrate to the solid tumors because of their small sizes (Van Audenhove and Gettemans, 2016). However, similar to other small-sized therapeutic proteins, they require high-dose administration and/or repeated injections to reach the therapeutic window in the circulation. This is caused by a rapid clearance via glomerular filtration that affects the treatment efficacy, patient compliance, and bystander effects (Ahmadpour and Hosseini-mehr, 2018). Several strategies have been developed to extend the plasma half-life of small therapeutic proteins (Dingermann, 2013; Brandl et al., 2019). Polyethylene glycol (PEG)-ylation is a successful strategy because several PEGylated biopharmaceuticals are currently approved and available in the market (Brandl et al., 2019). The noticeable features of PEG, high hydrophilicity, and random coil conformation in the aquatic environments increase the hydrodynamic radius of protein above the renal filtration threshold (6–8 nm) (Longmire et al., 2008; Cohan et al., 2011). However, despite there being many available PEGylated drugs in the market, PEGylation technology has several disadvantages, including accumulation of PEG polymer in the kidney, high cost of production, high polydispersity, nonbiodegradability, tendency to raise neutralizing anti-PEG antibodies, high viscosity in PEG formulations, and difficult manufacturing processing (Gebauer and Skerra, 2018). Recently, PEG mimetic peptides have been developed based on recombinant DNA technology. It extends the half-life of small-sized biopharmaceuticals in the circulation similar to PEG without problems associated with PEG polymer. Although initially designed PEG mimetic peptides had deleterious effects on the biologic activity and solubility of fused protein (Kontermann, 2012; Schmidt, 2013), recent advances led to design of peptide sequences without the mentioned problems. In the last developed technology, proline, alanine, serine (PAS)-ylation, a hydrophilic random coil sequence of proline, alanine, and serine repeats (100–600 amino acids) was genetically fused either to the N terminus or C terminus of desired protein (Ahmadpour and Hosseini-mehr, 2018). In contrast with albumin and Fc fusion technologies, desired pharmacokinetic parameters can be achieved in a controlled manner (Kontermann, 2012). Moreover, the PAS sequence provides monodisperse fusion proteins with a definite size and unique pharmacokinetic profile. Designed PAS sequences are nonimmunogenic, fully biodegradable, highly soluble, without accumulation in normal organs, resistant to the plasma proteases, easily produced in prokaryotic systems, and of a random coil structure without negative or positive charges (Schellenberger et al., 2009; Schlapschky et al., 2013; Podust et al., 2016; Gebauer and Skerra, 2018).

In the current study, for the first time, a novel PAS sequence, called PAS#208, was employed to extend the plasma

half-life of a nanosized anti-VEGFA single-domain antibody. The physicochemical properties, *in vitro* biologic activity, as well as pharmacokinetic parameters of the developed PASylated nanobody were compared with the native protein.

## Materials and Methods

**Chemical Reagents and Media.** Anti-VEGFA nanobody in pHEN6 expression plasmid was gifted from Department of Biotechnology, Pasteur Institute of Iran. Recombinant human VEGFA165 (rhVEGFA<sub>165</sub>) and HRP-conjugated anti-His antibody were purchased from R&D Systems (Minneapolis, MN) and Roche (Basel, Switzerland), respectively. All other chemicals were obtained from Merck (Darmstadt, Germany). MDA-MB-231 and human embryonic kidney 293 (HEK293) cells were purchased from the national cell bank (Pasteur Institute of Iran) and cultured in Dulbecco's modified Eagle's medium supplemented with 2% FBS in a 37°C incubator with 5% CO<sub>2</sub>. Female BALB/c mice (20 g in weight) were also obtained from Pasteur Institute of Iran, and animal study was in accordance with the Helsinki Declaration.

**Design of PAS#208 Sequence.** We checked several previously reported PAS sequences, including PAS#1, PAS#2, PAS#3, PAS#4, PAS#5, and PAS#1P2, which are different in the percentage of proline, alanine, and serine amino acids as well as the order of residues. After structural investigation on how these amino acids could increase the volume of the molecule, we finally purposed APSPASPA sequence for enhancing the pharmacokinetic parameters of an anti-VEGF nanobody. A computational method was used to check the volume of PAS#208 before the experimental step, which is essential for pharmacokinetic enhancement of small-sized therapeutic proteins (Kontermann, 2011). Briefly, the 3D-model of PAS#208 polypeptide was built by I-TASSER server (Roy et al., 2010). The generated model was then subjected to all-atom molecular dynamics simulation using all-atom optimized potentials for liquid simulations force-field GRO-MACS package version 2016.3 in a Linux Mint 17 operating system (Hess et al., 2008). The simulation was continued until the root-mean-square deviation of the protein was reached at a plateau. The 3D model was placed at the center of a cubic box with 1.0 nm from the boundary, and the periodic boundary condition was applied. An extended simple point charge (SPCE) model was used as a water model, and the system was neutralized by adding either Na<sup>+</sup> or Cl<sup>−</sup> ions. The temperature and pressure were kept at 300 K and one bar using Berendsen thermostat and Parrinello-Rahman barostat algorithms, respectively. Finally, the volume of PAS#208 polypeptide was measured using *gmx sasa* command.

**Expression and Purification of the Fusion Protein.** PAS#208 sequence was C-terminally fused to the anti-VEGFA nanobody. Moreover, a His-tag sequence was added to the C terminus of fusion protein for identification and purification. The construct was ordered to synthesize and clone into pET-26b(+) vector by Biomatik (Cambridge, Canada) using NdeI and EcoRI restriction enzymes. The expression plasmid was then transformed to BL21 (DE3) *Escherichia coli* strain using heat shock protocol. For protein expression, a positive clone was cultured in Terrific broth supplemented with 50 mg/ml kanamycin. The expression was induced by adding 1 mM isopropyl β-D-1-thiogalactopyranoside (OD<sub>600 nm</sub> = 0.5), and the culture was incubated for 16 hours at 30°C. The bacterial cells were then centrifuged at 12,000g for 5 minutes and disrupted by adding 2-[[2-hydroxy-1,1-bis(hydroxymethyl)ethyl]amino]ethanesulfonic acid buffer (0.5 M sucrose, 1 mM EDTA, and 0.1 M Tris/HCl, adjusted to pH 8.0). The fusion protein was purified using Ni-nitrilotriacetic acid affinity chromatography according to the instruction (Qiagen, Germany). The buffer was exchanged, and the protein was concentrated by ultrafiltration (3000 kDa cut-off; Millipore). Similar steps were done for the expression and purification of anti-VEGF nanobody. The expression of both proteins was studied by 15% SDS-PAGE and Coomassie Brilliant Blue staining method. For protein identification,

the lysates were blotted into nitrocellulose membranes (Bio-Rad, Hercules, CA) and then blocked by skim milk 2.5% in Tris-buffered saline/Tween 20 (0.02 M Tris, 0.5 M NaCl, 0.05% Tween20, adjusted to pH 7.4) overnight at 4°C. Thereafter, the blocked membranes were washed three times using Tris-buffered saline/Tween 20 buffer and incubated with anti-His HRP-conjugated antibody (1: 2000 dilution; Roche) for 1 hour at 37°C. Finally, the membranes were stained with 3,3'-diaminobenzidine (Sigma) according to the instructions. The protein concentrations in all steps were measured using Bradford assay (Bradford, 1976).

**Electrophoretic Mobility Assay.** PAGE (15%) and Coomassie Brilliant Blue staining method were used for electrophoretic mobility assessment of PASylated nanobody in comparison with the native protein. The electrophoretic mobility of purified proteins was defined as the distance traveled by the proteins through the polyacrylamide gel (Kim et al., 2006).

**Circular Dichroism Spectroscopy.** The change in the secondary structure of nanobody after fusion to the PAS#208 sequence was analyzed using a spectropolarimeter (JASCO Corporation, Tokyo, Japan). The spectra were recorded at 190–250 nm using 0.5 mg/ml protein solutions at room temperature (bandwidth 1 nm, scan speed 200 nm/min, response 1 second). Finally, the molar ellipticity (QM) was calculated for both proteins using the following equation:

$$QM = 1/4 Q_{obs} / (cd)$$

in which  $Q_{obs}$  is the measured ellipticity,  $c$  is the protein concentration (M), and  $d$  is the path length of the cuvette (cm) (Zvonova et al., 2017).

**Size Distribution and Zeta Potential.** Size distributions and zeta potential of nanobody after fusion to the PAS#208 sequence were measured using Zetasizer Nano ZS (Malvern) at a concentration of 0.3 mg/ml.

**Binding Potency.** The binding potency to rhVEGFA<sub>165</sub> was determined by a homemade ELISA. Briefly, 1 µg rhVEGFA<sub>165</sub> was coated in each well, and the wells were blocked with skim milk solution (3% w/v in PBS) for 1 hour at RT. After being washed three times with PBS/Tween, different concentrations of nanobody and the fused form were added, and the plates were further incubated for 1 hour at RT. The plates were then washed with PBS/Tween and incubated with anti-His HRP-conjugated antibody (1:2000 dilution; Roche) for 1 hour at RT. Finally, the substrate (3,3',5,5'-tetramethylbenzidine; PishtazTeb, Iran) was added, and the absorbance was measured at a wavelength of 450 nm using a spectrophotometer (BioTeK). Four-parameter logistic regression method was used for curve fitting. The EC<sub>50</sub> values were calculated by Prism 8 software (GraphPad Software) after curve fitting.

**VEGFA Neutralization.** VEGFA neutralization was assessed on MDA-MB-231 cells in vitro. HEK293 cells were also used as a VEGFR2 negative cell line. Different concentrations of nanobody and the PAS#208 fused form were incubated with 50 ng/ml rhVEGFA<sub>165</sub> for 4 hours at 37°C. The mixtures were then added to the cultured cells and incubated for 72 hours. After incubation, 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyl tetrazolium bromide solution (5 mg/ml) was added to each well and incubated for 4 hours at 37°C. The crystalline dye was finally solubilized by adding DMSO, and the absorbance was measured at a wavelength of 570 nm using a spectrophotometer (BioTeK). Two-way ANOVA was used for statistical analysis of VEGF-neutralizing assay.

**Pharmacokinetic Study.** BALB/c mice were randomly divided into two groups (nanobody and PASylated nanobody,  $n = 24$ ) and received an intravenous dose of 5 mg protein/kg. The blood samples were collected after 5, 15, and 30 minutes and 1, 2, 3, 4, 5, 6, 8, 24, 48, and 72 hours of injection. The plasma was taken by centrifugation at 12,000g for 25 minutes at 4°C. The protein concentrations were measured by a homemade ELISA as previously described. The plasma from PBS-receiving mice was used as blank. A two-phase decay regression method was used for the curve fitting. The terminal

half-life ( $T_{1/2}$ ) was determined using linear regression of the last three plasma concentrations. The mean area under the curve ( $AUC_{0-\infty}$ ) was determined using a linear trapezoidal method with extrapolation to infinity. Clearance (CL) and volume of distribution ( $V_d$ ) values were also calculated (Cohan et al., 2011; Maleki et al., 2012).

**Statistical Analysis.** Curve plotting and data analysis were carried out using Prism 8 (GraphPad Software). A  $P$  value of less than 0.05 was considered a statistically significant difference between the groups.

## Results

**Design of PAS#208 Sequence.** The 3D model of PAS#208 polypeptide was generated, and the molecular dynamics were investigated in an aqueous solution for 100 ns (Fig. 1). The proposed PAS#208 sequence had a volume of 18,205 Å<sup>3</sup>, which was comparable to that of previously reported PAS sequences (Skerra et al., 2013).

**Electrophoretic Mobility.** Periplasmic PAS#208-Nb and nanobody were purified using nickel affinity chromatography. The electrophoretic assessment on 15% gel showed lower mobility of PASylated nanobody at ~75 kDa (Fig. 2A). A band around 15 kDa was observed in the gel for nanobody. The identification of PAS#208-Nb was performed using an anti-His monoclonal antibody (Fig. 2B).

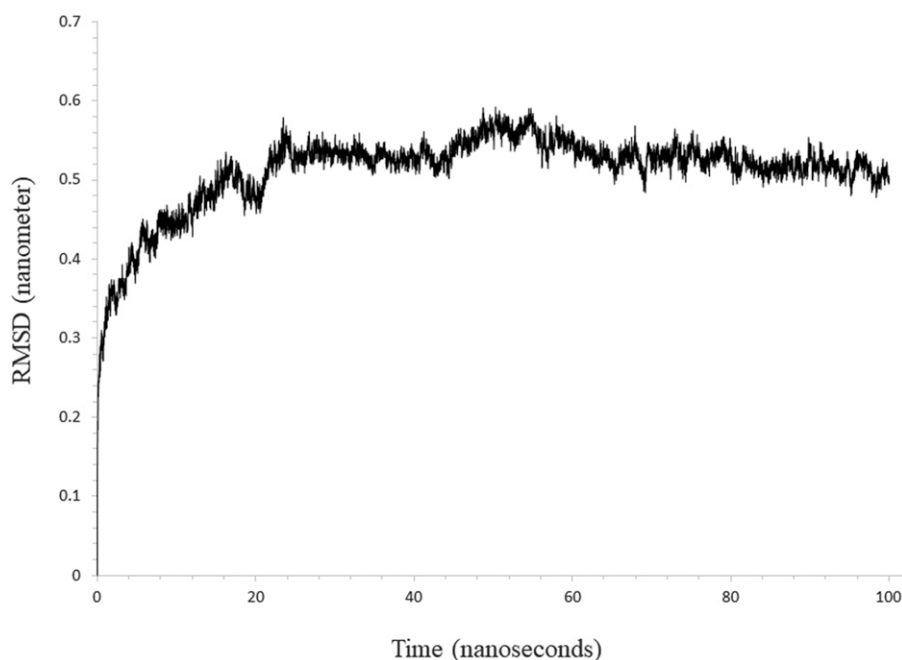
**Size Distribution and Zeta Potential.** The hydrodynamic radius and zeta potential of PAS#208-Nb were studied using dynamic light scattering and electrophoretic light scattering, respectively. The hydrodynamic radius of nanobody increased 5.3-fold by the attachment of PAS#208 sequence (Fig. 3). Size distribution analysis showed peaks at 77 nm (Khodabakhsh et al., 2018) and 409 nm for the native and the PASylated form, respectively. In contrast, no significant difference was observed in zeta potential after the PAS#208 fusion. The observed values were −2.8 and −2.4 mV for PAS#208-Nb and nanobody, respectively.

**Secondary Structure.** The secondary structure of the proteins was studied using circular dichroism spectroscopy. Molar ellipticity was calculated and plotted against wavelengths. A negative shift was observed for PAS#208-Nb in the spectrum at a wavelength of 204 nm (Fig. 4), indicating an increase in random coil conformation of the protein.

**Binding Potency.** The binding potency of nanobody after fusion to PAS#208 was determined by a homemade ELISA. After curve fitting, the EC<sub>50</sub> values were calculated as  $2.01 \times 10^{-7}$  and  $1.76 \times 10^{-5}$  M for PAS#208-Nb and nanobody, respectively. The data revealed that the PAS#208 sequence positively affects the antigen-binding potency of nanobody with a saturation state at lower concentrations (Fig. 5).

**VEGFA Neutralization.** VEGFA neutralization of PAS#208-Nb and nanobody were investigated on MDA-MB-231 breast-cancer cells. HEK293 cells were used as a control because of a lack of VEGFR2 expression. PAS#208-Nb and nanobody showed the same VEGFA-neutralizing effect on MDA-MB-231 breast-cancer cells (Fig. 6A). These data indicated that PAS#208 did not have a deleterious effect on the neutralizing efficacy of nanobody. In addition, all proteins did not show any effect on HEK293 because of lacking VEGFR2 even after 72 hours treatment (Fig. 6B).

**Pharmacokinetics.** The plasma concentration of the proteins was determined at defined time intervals, and a two-phase decay model was used for curve fitting of data (Fig. 7).



**Fig. 1.** Root-mean-square deviations (RMSDs) of PAS#208 polypeptide during 100 nanoseconds molecular dynamics simulation.

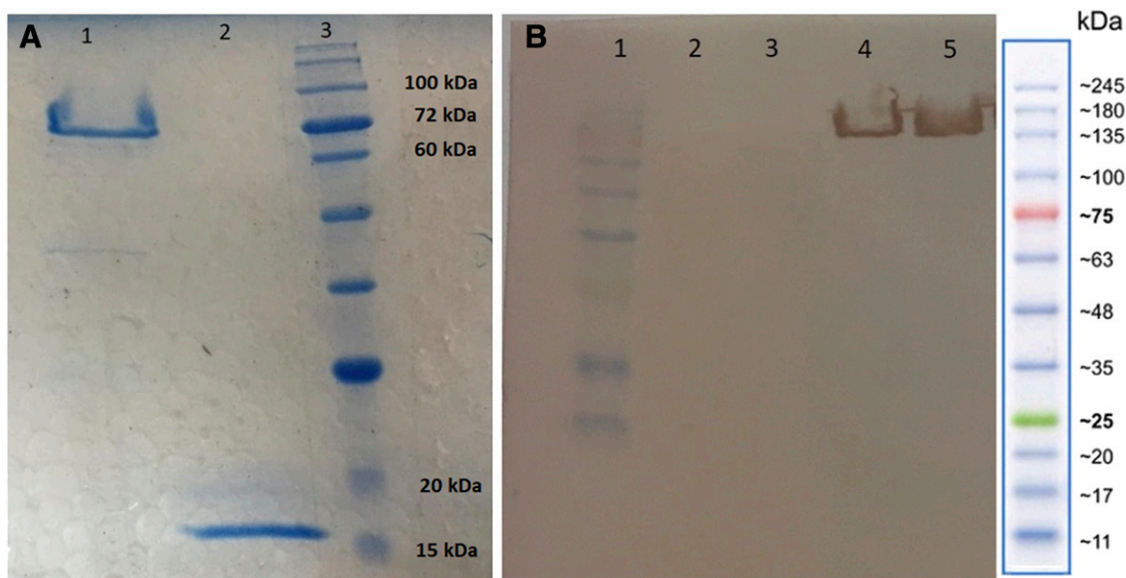
Pharmacokinetic parameters, including  $T_{1/2}$ , the  $V_d$ , elimination rate constant ( $\beta$ ), and CL, were calculated. The terminal half-life of PAS#208-Nb was increased 14-fold in comparison with the native protein. Moreover,  $V_d$ , CL,  $\beta$ , and AUC parameters were enhanced for the PASylated nanobody by 0.01-, 0.06-, 0.07-, and 24.1-fold, respectively (Table 1).

## Discussion

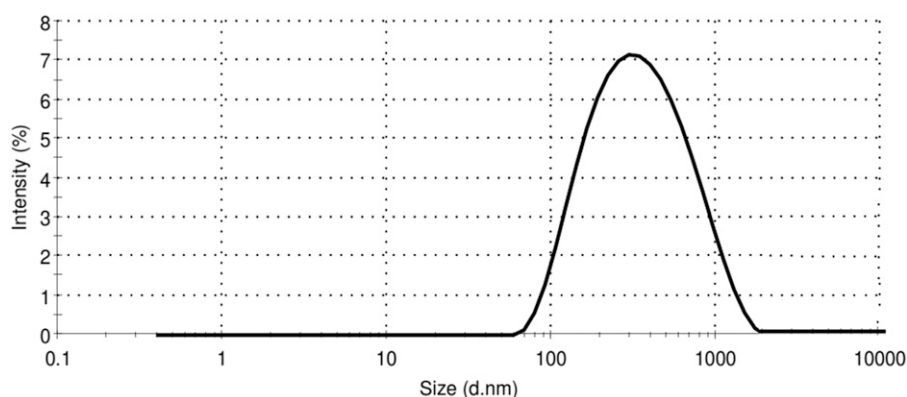
Despite several advantages of antibody fragments, very short in vivo half-life is a critical point to apply them popularly in the clinic. To overcome this obstacle, different strategies have been developed. Recently, a new promising strategy called PASylation genetically links repeats of unstructured

sequences of proline, alanine, serine to the gene of interest and remarkably enhances the pharmacokinetic parameters in vivo by a reduction in glomerular filtration rate (Skerra et al., 2013). Moreover, it can be easily established in the prokaryotic expression systems because it has no need for post-translational modifications (Schlapschy et al., 2013).

In the current study, for the first time, we designed a new PAS sequence called PAS#208. Then, physicochemic and in vitro biologic characteristics and in vivo pharmacokinetic parameters were tested by the fusion to an anti-VEGF single-domain antibody. Similar to PAS#1(200) sequence, the deigned PAS#208 noticeably improved the physicochemic properties of the fused fragmented antibody. Because of the hydrophilic nature of the PAS#208 sequence, like other same length PAS



**Fig. 2.** (A) Electrophoretic mobility of purified PAS#208-Nb and nanobody on 15% gel (lane 1: nanobody; lane 2: PAS#208-Nb; lane 3: marker). (B) Western blot analysis of PAS#208-Nb (lane 1: marker; lanes 2 to 3: PAS#208-Nb clones before induction; lanes 4 to 5: PAS#208-Nb clones after induction with 1 mM isopropyl  $\beta$ -D-1-thiogalactopyranoside).



**Fig. 3.** Size distribution analysis of PAS#208-Nb using dynamic light scattering technique.

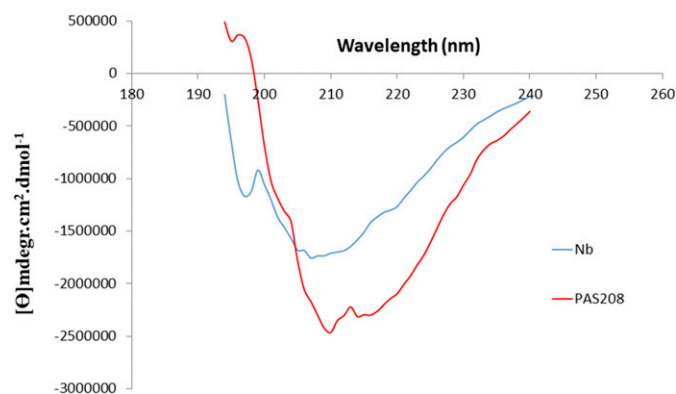
sequences, the electrophoretic mobility of fusion protein showed a 2-fold decrease in the electric field. This phenomenon can be explained by the lower binding affinity between the hydrophobic SDS and hydrophilic PAS#208 sequence in the polyacrylamide gel electrophoresis. As shown, the negative charge of SDS is the main driving force for the mobility of proteins in the gel networks (Schlapschy et al., 2013; Zvonova et al., 2017). Moreover, lower electrophoretic mobility can also be related to the unstructured nature of the PAS#208 sequence. As revealed by circular dichroism, an increase in random coil structure was observed similar to the other investigations on PAS#1 sequence. This highly flexible random conformation subsequently increases the occupied volume of the fusion protein in water, which makes it harder to pass through the pores of the gel (Schlapschy et al., 2013; Morath et al., 2015; Zvonova et al., 2017).

Size distribution measurement revealed a great increase in the hydrodynamic radius of the protein after the fusion to PAS#208. However, in contrast to Fc or albumin fusion technologies, it did not limit the penetration rate of the drugs into the targeted tissues because of the high flexibility as well as the controllable size of PAS sequences. In addition, a lower aggregation rate was observed in comparison with the native protein. The exposure of polar groups like hydroxyl groups of serine residues as well as other atoms that can be involved in donor or acceptor hydrogen binding in the PAS#208 sequence can explain the lower aggregation rate (Schlapschy et al., 2013). Zeta potential measurement indicated PAS#208 fusion did not change the net charge of the native protein, which was similar to our previous data obtained by the fusion of PAS#1(200) to the anti-VEGF single-domain antibody (Khodabakhsh et al., 2018). Similar observations were also reported by other studies that PAS sequences did not alter the charge because no ionizing groups exist in the designed PAS sequences (Schlapschy et al., 2013). This is very important in the manufacturing of PASylated proteins because no variation is needed for downstream processes, which prevent additional costs in the production. Additionally, it was shown that the coupling of negative or positive moieties to the drugs severely affects the drug distribution as well as affinity to the receptor like glutamic acid-rich sequences (XTEN moiety) (Schlapschy et al., 2013).

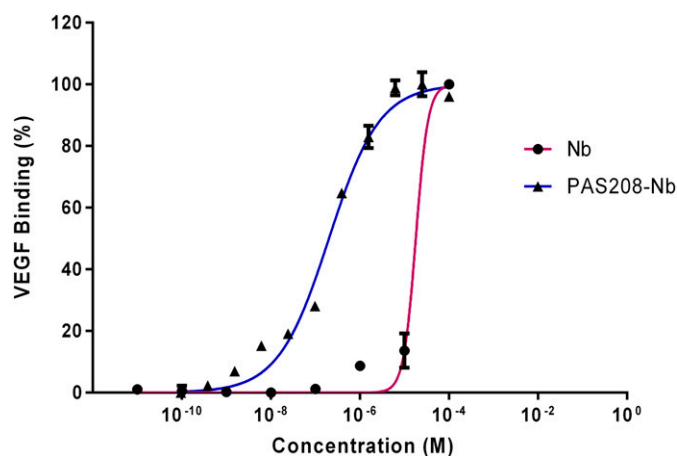
Similar to other investigations on different PAS sequences, molecular simulations revealed the PAS#208 sequence shows a random coil conformation without deleterious effects on the secondary structure of nanobody, which was experimentally confirmed by circular dichroism. This random coil structure

did not affect the receptor-binding site of the native protein after the C terminus fusion to PAS#208 as shown by the binding potency test. Because the PAS#208 sequence acts as a flexible linker, no linker is necessary to fuse this sequence to the desired proteins to keep the affinity. Other half-life extension technologies often reduce the binding affinity of the native protein.

Although major changes were made in the physicochemical characteristics of PAS#208-Nb, *in vitro* antiproliferative activity of the native remained intact after the fusion to PAS#208. Nanobody and PAS#208-Nb could equally inhibit the propagation of breast-cancer cells (MDA-MB-231) expressing VEGFR2 on the cell surface. These results are similar to those from our study on this protein that fused to PAS#1(200) sequence. Similarly, nanobody and PAS#208-Nb did not show any cytotoxicity on HEK293 cells because no VEGFR2 expression was found on the cell surface (Khodabakhsh et al., 2018). Different technologies were developed to compensate for the short *in vivo* half-life of miniaturized antibodies for medicinal purposes, such as antialbumin nanobody conjugation, PEGylation, and biodimerization (Vugmeyster et al., 2012; Hoefman et al., 2015; Van Roy et al., 2015). However, these approaches usually have unpredictable/deleterious effects on the physicochemical or biologic properties of the desired protein. In addition, in some cases, these approaches are usually hard to establish at the industrial scale and include difficult manufacturing processes. Long-acting biopharmaceuticals can easily produce by PASylation technology that improves the pharmacokinetic parameters of protein in a controlled manner by adding repeated sequences at the genetic level

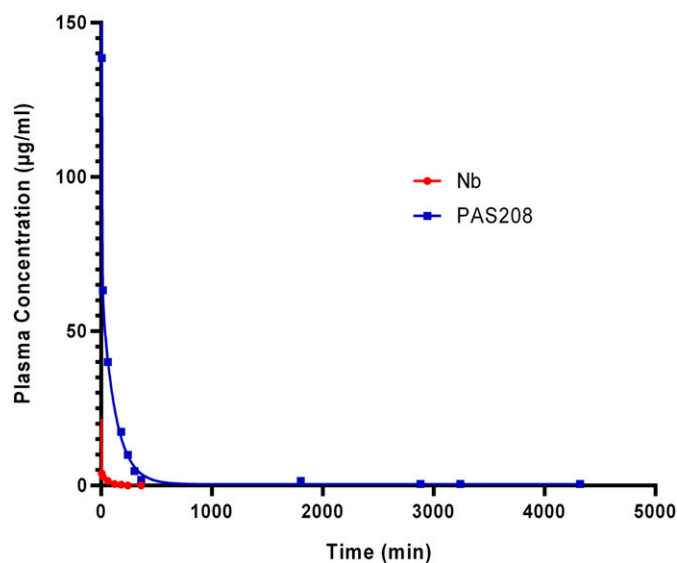


**Fig. 4.** Secondary structure analysis of PASylated nanobody and the native protein.



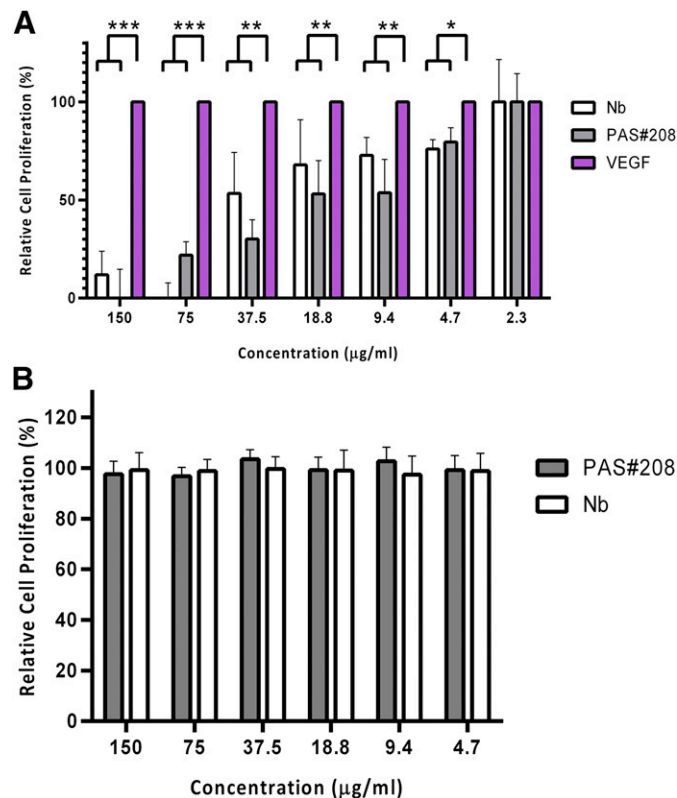
**Fig. 5.** Binding potency measurement. Data are presented as mean  $\pm$  S.D. from three independent measurements.

without an extra downstream process or undesired effects on the native protein. As shown in our previous study, PAS#208 also significantly increased the  $T_{1/2}$  of the native protein by a factor of 14 after a single dose intravenous administration. Similar to PAS#1(200)-Nb, the pharmacokinetic profile of PAS#208-Nb showed a slower biexponential decay than the native protein. This phenomenon can be explained by random chain behavior of PAS#208 sequence and an increase in the hydrodynamic volume of nanobody after fusion to PAS#208



**Fig. 7.** Pharmacokinetic behavior of PAS#208-Nb and the native protein after an intravenous injection of 5 mg/kg protein in mice. Nanobody was not measured in the plasma after 6 hours, whereas PAS#208-Nb was detectable in the circulation even at 72-hour follow-up.

sequence that leads to lower glomerular filtration rate in the kidney. Such pharmacokinetic enhancements were also observed in PAS#1(200) in our previous studies (Hedayati et al., 2017; Khodabakhsh et al., 2018). The residence of the protein in the circulation and high permeability into tumor tissues increases in-site drug concentration and enhances the efficacy of treatment.



**Fig. 6.** VEGFA neutralization of PAS#208-Nb and nanobody on (A) MDA-MB-231 and (B) HEK293. Data are presented as mean  $\pm$  S.D. from three independent measurements. The asterisks indicate the level of significance between groups (\*\* $P < 0.001$ ; \*\* $P < 0.01$ ; \* $P < 0.05$ ).

## Conclusion

In the current study, for the first time, we developed a new PAS sequence that has comparable physicochemical, biologic, and pharmacokinetic features to the previously reported PAS#1(200) sequence. The in vitro data of our study indicated that, despite adding PAS#208 sequence to the nanobody at the gene level, this sequence did not show any deleterious effect on the binding potency as well as neutralizing activity of the native protein. Moreover, this sequence had no cytotoxicity on the normal cells used in the study. Surprisingly, after just one dose administration of PAS#208-Nb to the mice, the sequence remarkably improved pharmacokinetic parameters, including terminal half-life, AUC, and the volume of distribution as well as clearance due to an increase in the hydrodynamic volume of the native protein. The simplicity as well as superior effects on half-life extension make PAS#208 sequence a novel sequence for in vivo pharmacokinetic enhancement of recombinant small proteins.

**TABLE 1**  
Pharmacokinetic parameters of PAS#208-Nb and the native protein calculated by the linear trapezoidal method

Protein	$T_{1/2}$ (min)	$[AUC]_{0-\infty}$ ( $\mu\text{g} \cdot \text{min}/\text{ml}$ )	$V_d$ (ml)	Clearance ( $\text{ml}/\text{min}$ )	Elimination Rate Constant ( $\beta$ ) ( $\text{min}^{-1}$ )	PK Factor
Nanobody	49	483	30.4	0.006815	0.014	1
PAS#208-Nb	693	11,630	0.4	0.000402	0.001	14

## Acknowledgments

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## Authorship Contributions

*Participated in research design:* Khodabakhsh, Cohan.

*Conducted experiments:* Khodabakhsh, Mehdizadeh, Khosravy, Vafabakhsh, Karami, Cohan.

*Performed data analysis:* Khodabakhsh, Salimian, Cohan.

*Wrote or contributed to the writing of the manuscript:* Khodabakhsh, Salimian, Cohan.

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