Mechanistic Multi—Tissue Modeling of Glucocorticoid-Induced Leucine Zipper Regulation: Integrating Circadian Gene Expression with Receptor-Mediated Corticosteroid Pharmacodynamics

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ABSTRACT

The glucocorticoid-induced leucine zipper (GILZ) is an important mediator of anti-inflammatory corticosteroid action. The pharmacokinetic/pharmacodynamic/pharmacogenomic effects of acute and chronic methylprednisolone (MPL) dosing on the tissue-specific dynamics of GILZ expression were examined in rats. A mechanism-based model was developed to investigate and integrate the role of MPL and circadian rhythms on the transcriptional enhancement of GILZ in multiple tissues. Animals received a single 50-mg/kg intramuscular bolus or a 7-day 0.3-mg/kg/h subcutaneous infusion of MPL and were euthanized at several time points. An additional group of rats were euthanized at several times and served as 24-hour light/dark (circadian) controls. Plasma MPL and corticosterone concentrations were measured by high-performance liquid chromatography. The expression of GILZ and glucocorticoid receptor (GR) mRNA was quantified in tissues using quantitative real-time reverse-transcription polymerase chain reaction. The pharmacokinetics of MPL were described using a two-compartment model. Mild-to-robust circadian oscillations in GR and GILZ mRNA expression were characterized in muscle, lung, and adipose tissues and modeled using Fourier harmonic functions. Acute MPL dosing caused significant down-regulation (40%–80%) in GR mRNA and enhancement of GILZ mRNA expression (500%–1080%) in the tissues examined. While GILZ returned to its rhythmic baseline following acute dosing, a new steady-state was observed upon enhancement by chronic dosing. The model captured the complex dynamics in all tissues for both dosing regimens. The model quantitatively integrates physiologic mechanisms, such as circadian processes and GR tolerance phenomena, which control the tissue-specific regulation of GILZ by corticosteroids. These studies characterize GILZ as a pharmacodynamic marker of corticosteroid actions in several tissues.

One such gene that is highly regulated by CS is the glucocorticoid-induced leucine zipper (GILZ). GILZ has emerged as an important mediator of the anti-inflammatory actions of CS (Ayroldi and Riccardi, 2009). Its major mechanism of action involves binding to the p65 subunit of NFkB (Di Marco et al., 2007), thereby repressing its translocation into the nucleus and consequent proinflammatory gene expression. Recent evidence also demonstrates its role in modulating tumor growth and cell proliferation (Ayroldi et al., 2015; Bruscoli et al., 2015). Therefore, pharmacologic enhancement of GILZ will influence CS therapy.

Many CS-regulated genes, including GILZ, have been previously examined. However, most studies were performed in vitro and, hence, are unable to provide holistic information regarding underlying systemic and tissue-specific processes. Furthermore, little is known regarding the temporal patterns of CS-regulated genes in vivo and their governing mechanisms. Development of mechanistic pharmacokinetic (PK) and pharmacodynamic (PD) models is essential for gaining quantitative understanding of the physiologic and pharmacological mechanisms underlying the time course of diverse drug responses.

ABBREVIATIONS: ADX, adrenalectomized; CS, corticosteroid; CST, corticosterone; CV, coefficient of variation; GILZ, glucocorticoid-induced leucine zipper; GR, glucocorticoid receptor; GRE, glucocorticoid-response element; IC, initial conditions; IDR, indirect response; MPL, methylprednisolone; PD, pharmacodynamic; PEPCK, phosphoenolpyruvate carboxylase; PK, pharmacokinetic; qRT-PCR, quantitative real-time reverse-transcription polymerase chain reaction; TAT, tyrosine aminotransferase.
Such PK/PD models have been developed in our laboratory to describe the receptor/gene-mediated effects of steroids on target genes, such as tyrosine aminotransferase (TAT) (Ramakrishnan et al., 2002a), glutamine synthetase (Sun et al., 1999), and phosphoenolpyruvate carboxylase (PEPCK) (Jin et al., 2004), in adrenalectomized (ADX) rats.

Although TAT, glutamine synthetase, and PEPCK are useful biomarkers to probe the genomic effects of CS, they share a common limitation—in vivo expression is confined to one or two tissues. The rate-limiting enzyme in tyrosine metabolism, TAT, lacks a direct clinical relevance. PEPCK, which catalyzes the rate-limiting step of gluconeogenesis, is regulated by various hormones, including CS, glucagon, and insulin, confounding the simple assessment of CS effects alone. In contrast, several features make GILZ a robust marker to investigate CS sensitivity. First, GILZ is ubiquitously expressed in multiple tissues in humans and in the rat (Cannarile et al., 2001; Ayyar et al., 2015). Second, GILZ shows exquisite sensitivity to enhancement by CS due to the presence of multiple functional glucocorticoid-response elements (GREs) in its 5′-upstream promoter region (van der Laan et al., 2008). Finally, GILZ expression is, at least in part, directly related to the anti-inflammatory efficacy of CS.

Since adrenal release of endogenous glucocorticoid hormones occurs in a rhythmic manner, their downstream target genes in peripheral tissues may be expected to follow similar oscillations. Indeed, many steroid-regulated genes, including cholesterol-7a-hydroxylase, TAT, and GR, exhibit circadian rhythms (Van Cantfort and Gielen, 1979; Sukumaran et al., 2010). GILZ also demonstrates a circadian rhythm in vivo, which is entrained to that of plasma corticosterone (CST) in rats (Ayyar et al., 2015). Such circadian responses add time-dependent complexities (Jusko, 1995), which must be accounted for while evaluating drug effects.

We developed and applied a mechanism-based PK/PD/pharmacogenomic model with circadian-controlled processes that describes the tissue-specific dynamics of GILZ mRNA expression in skeletal muscle, lung, and white adipose tissue. The GILZ and GR mRNA dynamics were examined in intact (non-ADX) rats to evaluate concerted effects of circadian rhythms and CS pharmacodynamics. The mechanistic model was fitted simultaneously to data from un-treated and single-dosed animals to yield tissue-specific information on drug- and system-specific parameters. Simulations were performed to predict the GILZ mRNA dynamics in lung and adipose tissue upon chronic dosing and to gain new insights into the tissue- and dose regimen–dependent aspects controlling receptor-mediated gene expression in vivo. Collectively, these studies provide a quantitative and mechanistic framework for the application of GILZ as a PD marker of a CS anti-inflammatory mediator in tissues of clinical relevance.

Materials and Methods

Animals

Experiments used tissue samples harvested from three separate population-based animal studies conducted in our laboratory. An extensive description of these studies can be found in previously published reports (Hazra et al., 2007a; Almon et al., 2008; Ayyar et al., 2015). Brief descriptions of the studies are provided here. In all studies, normal male Wistar rats were acclimated and housed under a 12-hour-12-hour light-dark cycle and constant-temperature (22°C) environment, with free access to drinking water and standard rat chow. All animals were housed in separate cages to facilitate animal manipulations while minimizing stress to the animals. The rats were euthanized by aortic exsanguination under ketamine/xylazine anesthesia (80:10 mg/kg). Blood samples were harvested using EDTA as an anticoagulant. Plasma was prepared from blood by centrifugation (200g, 4°C, 15 minutes), aliquoted, and stored at −80°C until further analyses. Several tissues, including abdominal adipose, lung, and skeletal muscle, were rapidly excised, flash frozen in liquid nitrogen, and stored at −80°C. Animals euthanized at the same time point were treated as triplicate measurements in each study. All animal study protocols adhered to the “Guide for the Care and Use of Laboratory Animals, 8th Edition” and were approved by the State University of New York at Buffalo Institutional Animal Care and Use Committee.

Experimental

Circadian Study. Fifty-four normal male Wistar rats purchased from Harlan Laboratories (Indianapolis, IN) were housed and allowed to acclimatize in a room equipped with a 12-hour light/dark cycle, and were subject to minimal environmental disturbance. Animals were euthanized by exsanguination on three successive days at 18 different time points ranging from 15 minutes to 23.75 hours after lights went on (n = 3 animals per time point).

Single Methylprednisolone Bolus Study. Sixty normal male Wistar rats purchased from Harlan Laboratories were used. Each animal was given a single 50-mg/kg IM bolus dose of methylprednisolone sodium succinate (Solu-Medrol; Upjohn, Kalamazoo, MI) in the left hind haunch between 1.5 and 3 hours after lights on (i.e., at the nadir of the circadian pattern of the endogenous CST rhythm). Animals were euthanized at 18 different time points ranging from 15 minutes to 4 days (96 hours) after receiving methylprednisolone (MPL) injection (n = 3 animals per time point). Control animals were euthanized in triplicate at 12 and 24 hours after saline injection.

Chronic MPL Infusion Study. Thirty-nine normal male Wistar rats were purchased from Harlan-Sprague Dawley Inc. (Indianapolis, IN). The treatment group (n = 27) were given 0.3 mg/kg/h methylprednisolone sodium succinate (Solu-Medrol) via SC implanted Alzet osmotic minipumps (Model 2001; Alza, Palo Alto, CA). Animals in the control group (n = 12) were implanted with vehicle-filled pumps. MPL-dosed animals were euthanized over 7 days following pump implantation (n = 3 animals per time point). Vehicle controls were euthanized at 6, 12, 18, and 24 hours after pump implantation (n = 3 animals per time point).

Drug and Endogenous Steroid Assay

Plasma CST and MPL concentrations were determined by a normal-phase high-performance liquid chromatography method (Haughey and Jusko, 1988). The limit of quantitation was 5 ng/ml for CST and 10 ng/ml for MPL. The interday and intraday coefficients of variation (CVs) were less than 10%.

RNA Preparation

Frozen tissue samples were ground into a fine powder under liquid nitrogen. Powdered samples were weighed, added to prechilled TRI Reagent (Invitrogen, Carlsbad, CA), and homogenized. Total RNA extractions were carried out using TRI Reagent and further purified by passage through RNeasy minicolumns (Qiagen, Valencia, CA) according to the manufacturer’s protocols for RNA cleanup. The RNA concentrations were quantified spectrophotometrically (NanoDrop 2000c; Thermo Fisher Scientific, Waltham, MA), and purity and integrity were assessed by agarose-formaldehyde gel electrophoresis. All samples exhibited 260/280 absorbance ratios of approximately 2.0, and all showed intact ribosomal 28S and 18S RNA bands in
an approximate ratio of 2:1 as visualized by ethidium bromide staining. Final total RNA preparations were diluted to desired concentrations in nucleic-free water (Ambion, Austin, TX) and stored in nucleic-free tubes at −80°C until use.

Quantification of mRNA Expression

The GILZ- and GR-specific quantitative real-time reverse transcription polymerase chain reaction (qRT-PCR) assays were developed and validated according to the Minimum Information for Publication of Quantitative Real-Time PCR Experiments guidelines (Bustin et al., 2009). Both qRT-PCR assays involved use of in vitro transcribed cRNA standards, gene-specific TaqMan-based probes, and a single-step assay. An extensive description of the subcloning and construction of the in vitro transcribed cRNA standards was reported previously (Ayyar et al., 2015). Primer and probe sequences were designed and custom-synthesized (Biosearch Technologies, Novato, CA). qRT-PCR was performed using a Brilliant qRT-PCR Core Reagent Kit, 1-Step (Stratagene, La Jolla, CA) in a Stratagene MX3005P thermocycler according to the manufacturer’s instructions. Primer and probe sequences were as follows: GR, forward primer 5′-AACATGTTGAGTGCCGTCGCA-3′, reverse primer 5′-GGTGTAGTTCACCCGATG-3′, and label probe 5′-capping, splicing, and 3′-polyadenylation to form mRNA, which are exported to the cytoplasm. mRNA transcripts—in this case, those encoding GILZ—are then translated into protein and/or degraded within the cytoplasm, leading to alterations in measurable mRNA and protein concentrations.

Pharmacokinetic/Pharmacodynamic/Pharmacogenomic Modeling

Pharmacokinetics. A two-compartment model with dual absorption pathways from the injection site was used to describe the PK of IM dosing of MPL (Hazra et al., 2007b). The PK parameters were fixed with estimates obtained from our previous study, as given in Table 1. Equations and initial conditions (IC) describing the model are:

\[
\begin{align*}
V_T \frac{dC_P}{dt} &= k_{a1} \cdot D_{(IM)} \cdot F \cdot F_r \cdot e^{-k_{a1} \cdot t} + k_{a2} \cdot D_{(IM)} \cdot F \cdot (1 - F_r) \cdot e^{-k_{a2} \cdot t} - CL \cdot C_P - CL_D \cdot C_P + CL_D \cdot C_T \quad IC = 0 \\
V_T \frac{dC_T}{dt} &= CL_D \cdot C_P - CL_D \cdot C_T \quad IC = 0
\end{align*}
\]

where \(C\) and \(D\) represent the concentration and dose of MPL in the corresponding plasma (P) and tissue (T) compartments, \(F\), and \(1 - F\) are fractions of dose absorbed through the absorption pathways described by first-order rate constants \(k_{a1}\) and \(k_{a2}\); \(CL\) is clearance from the central compartment, \(CL_D\) is the distribution clearance, \(F\) is the overall bioavailability of MPL after IM injection, and \(V_T\) and \(V_T\) are the central and peripheral volumes of distribution.

The same equations were used for the SC infusion kinetics, with the exception that a zero-order input function (0.3 mg/kg/h) was applied instead of the two first-order absorption terms. Distribution-related parameters (\(V_P\), \(V_T\), and \(CL_D\)) were fixed based on the bolus data, whereas the \(CL\) was estimated from the infusion data. The pharmacokinetic model schematic for both dosing regimens is depicted in Fig. 1. Plasma drug concentrations over time were fixed and used as a driving force for the dynamics in the subsequent data analysis.

Mechanistic Basis for Pharmacodynamics

The diverse cellular and molecular processes that govern the pharmacodynamic and pharmacogenomic effects of CS are depicted in Fig. 2. Approximately 77% of circulating CS in plasma is bound to corticosteroid-binding globulin (CBG) and albumin (Haughey and Jusko, 1992). Owing to its moderate lipophilicity, free (unbound) CS can passively diffuse across cell membranes into the cytosol, where the GR is located. Inactive GR is held and stabilized in the cytoplasm by molecular chaperones including heat shock proteins (hsp70 and hsp90) as well as the FK506-binding protein immunophils (Pratt and Toft, 1997). The CS bind to cytoplasmic GR and cause a dissociation of the chaperone complex by inducing a conformational change in the GR molecule. Upon dissociation from chaperone proteins, activated drug-receptor complexes rapidly translocate into the nucleus and homodimerize. The complexes then bind specific DNA sequences known as GREs in the 5′-upstream promoter regions of target genes, leading to transcriptional changes by altering the chromatin structure (Newton, 2000; Barnes, 2006) and consequent activation of the RNA-polymerase complex. This genome-level interaction positively or negatively regulates the expression of a plethora of genes. De novo synthesized RNA transcripts undergo 5′-capping, splicing, and 3′-Polyadenylation to form mRNA, which are exported to the cytoplasm. mRNA transcripts—in this case, those encoding GILZ—are then translated into protein and/or degraded within the cytoplasm, leading to alterations in measurable mRNA and protein concentrations.

After exerting their transcriptional effects, the steroid-receptor complexes in the nucleus may dissociate from GREs and return to the cytosol. Part of the receptors may be degraded during the process, whereas the rest may be reassembled with chaperone proteins and recycled. Therefore, the total pool of free cytosolic GR constitutes a composite of recycled and de novo synthesized GR molecules. Furthermore, the CS cause homologous down-regulation of their own receptors via decreased transcription, which subsequently results in decreased mRNA synthesis and free GR densities in the cytosol (Oakley and Cidlowski, 1993; DuBois et al., 1995).

Mathematical Model

Figure 3 depicts the integrated PK/PD/pharmacogenomic model that describes the tissue-specific effects of CS and circadian oscillations on the regulation of GILZ gene expression.

Glucocorticoid Receptor Dynamics

The dynamics of GR have been previously studied in liver and adipose tissue from normal male rats (Hazra et al., 2008; Sukumaran et al., 2011). Kinetic parameter values governing drug-receptor binding, translocation, and recycling were fixed to previously obtained values (Hazra et al., 2007a) since these processes are considered to be
similar across different tissues. The differential equations and initial conditions for GR dynamics in the tissues are:

\[
\frac{dR}{dt} = k_{s,GR} \times GR_m - k_{d,GR} \times R - k_{m} \times f_{mpt} \times C_{mpt} \times R + k_{c} \times DR_n \quad IC = R(0) \quad (3)
\]

\[
\frac{dDR}{dt} = k_{m} \times f_{mpt} \times C_{mpt} \times R - k_{c} \times DR \quad IC = DR(0) \quad (4)
\]

\[
\frac{dDR_n}{dt} = k_{c} \times DR - k_{rec} \times DR_n \quad IC = DR_n(0) \quad (5)
\]

where \( R \) is the free cytosolic receptor, \( DR \) is the cytosolic drug-receptor complex, and \( DR_n \) is the nuclear translocated drug-receptor complex concentrations. The rate constants include receptor synthesis \( (k_{s,GR}) \) and degradation \( (k_{d,GR}) \), translocation of the drug-receptor complex into the nucleus \( (k_c) \), the overall turnover of \( DR_n \) return receptors to cytosol \( (k_{rec}) \), as well as the second-order rate constant of drug-receptor association \( (k_{m}) \). Part of \( DR_n \) may recycle back to the cytosol controlled by the rate constant \( R_f \times k_{rec} \), and the rest is degraded with a rate constant \( (1 - R_f) \times k_{rec} \). The \( f_{mpt} \) is the unbound fraction of MPL in plasma.

The GR mRNA \( (GR_m) \) showed circadian oscillations in muscle, lung, and adipose, which were described using an indirect response (IDR) model with the mRNA synthesized by a time-dependent synthesis rate \( (k_{s,GRm}(t)) \) and degraded by first-order rate constant \( (k_{d,GRm}) \) as follows:

\[
\frac{dGR_m}{dt} = k_{s,GRm}(t) - k_{d,GRm} \times GR_m \quad IC = GR_m(0) \quad (6)
\]

The time-dependent synthesis rate of GR mRNA \( [k_{s,GRm}(t)] \) in adipose tissue was described using a two-harmonic function as

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Fig. 2. Schematic representation of diverse molecular and cellular mechanisms of corticosteroid action on regulating gene expression. CBG, corticosteroid-binding globulin; FKBP, FK506 binding protein; hsp 70/90, heat shock protein 70/90; nGRE, negative glucocorticoid response element; RNAP, RNA polymerase.

Fig. 3. PK/PD model schematic for the pharmacogenomic effects of corticosteroids and circadian rhythms on the transcriptional regulation of GILZ mRNA expression. Curved input represents circadian pattern in production, open boxes reflect stimulation, and solid boxes depict inhibition of production rate of a turnover process. The model is described by eqs. 3–12. Parameters are defined in Tables 2 and 3.
Circadian Rhythm of GILZ mRNA Expression

The GILZ mRNA displays circadian oscillations, which is under the complex regulation of CST as well as the peripheral circadian clock gene loop present in tissues (Aygar et al., 2015; Soták et al., 2016). Circadian rhythms in GILZ mRNA expression in tissues were modeled using an IDR model with a time-dependent synthesis rate \( k_{GILZm}(t) \), described by a single harmonic function and degraded by a first-order rate constant \( k_{d,GILZm} \) as:

\[
\frac{dGILZ_m}{dt} = k_{GILZm}(t) - k_{d,GILZm} \cdot GILZ_m \quad \text{IC} = GILZ_m(0)
\]

where \( a_i \) and \( b_i \) are Fourier coefficients associated with the harmonic oscillations. The values for these parameters were obtained by fitting the replicate GILZ mRNA expression data measured in tissues from the circadian control study using the FOURPHARM program (Kryzanowski et al., 2000).

Suppression in GR mRNA expression by MPL is given by:

\[
\frac{dGR_{m,mlp}}{dt} = k_{GRm,mlp}[1 - \left( \frac{DR_n}{DR_n + IC_{50,GRm}} \right)] - k_{d,GRm,mlp} \quad \text{IC} = GR_{m,mlp}(0)
\]

where the \( IC_{50,GRm} \) is the concentration of \( DR_n \) at which the synthesis rate of GR mRNA is reduced to 50% of its baseline. Measures of GR mRNA expression (\( GR_{m} \)) following MPL dosing in adipose tissue (Sukumaran et al., 2011), lung, and skeletal muscle were used to infer the concentrations of free cytosolic receptor density (\( R \)) in those tissues based on eq. (3).

Enhancement of GILZ mRNA Expression by CS

Transcriptional up-regulation of GILZ by CS has been documented in multiple cell types (D’Adamo et al., 1997; Eddleston et al., 2007; Aguilar et al., 2013). The pharmacogenomic effects of acute and chronic MPL dosing on GILZ mRNA expression in skeletal muscle, lung, and adipose tissue were modeled as a direct stimulation of the mRNA synthesis rate by the activated drug-receptor complex in the nucleus (\( DR_n \)) controlled by the stimulation constant, \( S_{DR_n,GILZm} \), as:

\[
d\frac{dGILZ_m,mlp}{dt} = k_{GILZm}(t) \left( 1 + S_{GILZm,mlp,DR_n} \right) - k_{d,GRm,mlp} \quad \text{IC} = GILZ_m,mlp(0)
\]

Data Analysis. The ADAPT 5 software was used for all data fitting and simulation of model equations (D’Argenio et al., 2009). The maximum likelihood method was applied for fitting the data. Replicate data at each time point from animals in each experiment were naïve-pooled, and data from both circadian control and single-dose experiments were modeled simultaneously. Replicate data from the chronic MPL infusion study served as an external model validation set. The goodness of fit was assessed by system convergence, visual inspection of the fitted curves, objective function values such as Akaike information criterion (AIC), improved likelihood, examination of residuals, and precision (CV%) of the estimated parameters. The following variance model was used for the model fitting:

\[
V_i = V(\theta, \sigma) = [\sigma_1 + 2\sigma_2 Y(\theta, t_i)] ^ 2
\]

where \( V(\sigma, \theta, t_i) \) is the variance for the \( i \)th point, \( Y(\theta, t_i) \) is the model-predicted value, \( \theta \) represents the estimated structural parameters, and \( \sigma_1 \) and \( \sigma_2 \) are the variance parameters that were estimated.

Animals in the dosing experiments were given MPL between 1.5 and 3 hours after lights on. For simplicity, the dosing time was assumed to be at circadian time 2.5 hours to compare the data obtained from both the MPL-dosing and circadian experiments. Hence, all pharmacodynamic profiles are plotted with respect to circadian time, with MPL given at 2.5 hours.

Results

Pharmacokinetics. The plasma concentration-time profiles of MPL following IM bolus and SC infusion regimes are shown in Fig. 4. The PK profile of IM dosed MPL was simulated using parameter estimates obtained from a previously conducted PK study (Hazra et al., 2007b). MPL is known to undergo nonlinear interconversion as well as extensive hepatic oxidative metabolism in rats (Kong and Jusko, 1991). Further, plasma protein binding is relatively constant (\( f_{imp} = 77\% \)) with concentration (Haughey and Jusko, 1992). Steady-state concentrations of MPL in the infusion study were roughly 100-fold lower compared with those in previous bolus studies (Sun et al., 1998; Hazra et al., 2007b). Therefore, \( CL \) was estimated from the infusion data. The first sampling time in the infusion study was at 6 hours after starting the infusion; by then, MPL had achieved steady-state concentrations. Thus, the rising phase of the PK profile, which provides information regarding drug absorption and distribution, was unavailable. Hence, the distribution clearance and volumes of distribution were fixed based on the previous bolus estimates (Hazra et al., 2007b). In addition, drug absorption from the SC site was assumed to be complete and rapid compared with the rate of drug release from the pump. MPL clearance increased from 4.0 to 8.3 l/h/kg, which suggests that high concentrations of MPL cause saturation of drug-metabolizing enzymes. The PK parameters describing the data for both dosing regimes are listed in Table 1.

Circadian Dynamics of GR mRNA Expression. The daily fluctuation of receptor mRNA was examined in skeletal muscle and lung obtained from normal animals housed under...
tightly controlled 12-hour light/12-hour dark cycles. The profile for adipose tissue was simulated based on previous data collected from the same set of animals (Sukumaran et al., 2011). The circadian dynamics of tissue-specific GR mRNA along with the model fittings are presented in Fig. 5.

Message expression in skeletal muscle (Fig. 5) showed a modest circadian rhythm, starting at $1164 \pm 66$ molecules/ng RNA in the light phase, with a nadir at the transition from the light to dark period (around 800 molecules/ng RNA) at 12 hours, before gradually increasing through the dark period. This pattern was well described by a single harmonic function. The baseline receptor mRNA expression was approximately 3-fold higher in lung compared with skeletal muscle (Fig. 5). Furthermore, lung GR exhibited a circadian pattern distinct from muscle, showing a nadir in the light phase at 7 hours and a peak in the dark phase around 18 hours, which was also adequately described by a single harmonic function. Interestingly, the observed patterns of receptor message in skeletal muscle and lung also varied from that observed in adipose tissue (Fig. 5), where the circadian oscillations peaked at the transition from the light to dark period at 12 hours, which was described by a two-harmonic Fourier function (Sukumaran et al., 2011).

**GR mRNA Dynamics upon Acute MPL Dosing.**

Dynamics of GR mRNA expression following acute CS dosing were measured in muscle and lung, and simulated in adipose tissue based upon a previous report (Sukumaran et al., 2011). The dynamics of GR mRNA suppression in each tissue along with the model fittings are shown in Fig. 6. MPL caused significant down-regulation in GR mRNA expression by 45% with the model fittings are shown in Fig. 6. MPL caused about 45%–50% suppression in muscle receptor mRNA expression was observed at the nadir after MPL dosing, which returned to the rhythmic baseline by 24 hours (Fig. 6). The estimated degradation-rate constant ($k_{d,GRm}$) value of 0.28 hour$^{-1}$ (29.9 CV%) in skeletal muscle was higher than the value of 0.14 hour$^{-1}$ reported in muscle from ADX rats (Sun et al., 1999). The nadir occurred around 7–8 hours after MPL versus 10–11 hours in the ADX rats, which could be attributed to the higher $k_{d,GRm}$ in the normal animals. Acute MPL dosing led to about 60% suppression in lung GR mRNA at the nadir around 7–9 hours and returned to baseline expression by 24 hours after MPL (Fig. 6), which was well described by the model. It can be noted that GR mRNA at the early time points in the treatment group was higher than expression observed upon return to baseline after MPL, which was similar to GR expression in the circadian controls. The estimated degradation-rate constant ($k_{d,GRm}$) value of 0.26 hour$^{-1}$ (15.4 CV%) was similar to that obtained in skeletal muscle (0.28 hour$^{-1}$) and in white adipose tissue (0.31 hour$^{-1}$) (Sukumaran et al., 2011), but lower than the reported value of 0.12 hour$^{-1}$ in liver (Hazra et al., 2007a). Furthermore, the nadir in receptor mRNA expression after MPL dosing was reached around the same time as in both muscle and adipose tissue, which could be attributed to similar $k_{d,GRm}$ values.

The suppression of GR mRNA expression by MPL in adipose tissue has been modeled previously (Sukumaran et al., 2011). Therefore, relevant parameter estimates were fixed to simulate the adipose tissue profile (Fig. 6). Tissue-specific rates of receptor synthesis ($k_{s,GR}$) and free cytosolic receptor densities at baseline [GR(0)] were also estimated using the dynamics of GR mRNA expression in the tissues. Table 2 provides the parameter estimates related to GR dynamics.

### Circadian Dynamics of GILZ mRNA Expression.

Endogenous cyclic regulation of GILZ mRNA expression was examined in skeletal muscle, lung, and adipose obtained from normal untreated animals. The dynamics of circadian oscillations in GILZ mRNA expression in all three tissues along with the model fittings are shown in Fig. 7. Superimposed on these figures is the profile of CST measured in plasma from the same animals. In all three tissues, GILZ mRNA regulation in vivo follows a pattern that is entrained to that of the CST rhythm.

Fig. 7 shows the circadian mRNA expression profile of GILZ in skeletal muscle. Interestingly, a prominent delay in peak (9330 ± 273 molecules/ng RNA) and trough (4350 ± 743 molecules/ng RNA) expression was observed compared to normal untreated animals. The dynamics of circadian oscillations in GILZ mRNA expression in all three tissues along with the model fittings are shown in Fig. 7. Superimposed on these figures is the profile of CST measured in plasma from the same animals. In all three tissues, GILZ mRNA regulation in vivo follows a pattern that is entrained to that of the CST rhythm.

![Fig. 4. MPL pharmacokinetics in rats. Simulated plasma concentrations versus time after 50 mg/kg intramuscular (IM) injection of MPL using eqs. 1 and 2. Pharmacokinetics of MPL upon administration of 0.3-mg/kg/h subcutaneous (SC) infusion for 7 days. Solid lines represent model fittings, circles depict the mean, and error bars depict 1 standard deviation (n = 3).](image-url)
with lung and adipose tissue (Fig. 7). Specifically, GILZ mRNA expression peaked at 20 hours and showed a nadir around 9–10 hours. The model well captured the trend of the circadian profile. In both lung and adipose, GILZ mRNA peaked in the dark period (18,867 ± 2347 molecules/ng RNA for adipose and 25,202 ± 1145 molecules/ng RNA for lung) at 16 hours and showed a trough in the light period (4446 ± 622 molecules/ng RNA for adipose and 5141 ± 615 molecules/ng RNA for lung) around 6–8 hours. Circadian rhythmicity in GILZ mRNA expression was strongest in lung compared with the other tissues. Although the model predicts peak expression around 17 hours, the data are captured reasonably well by the single Fourier harmonic function.

**GILZ mRNA Dynamics upon Acute MPL Dosing.** CS such as dexamethasone cause strong up-regulation of GILZ mRNA expression in vitro (D’Adamio et al., 1997; Smit et al., 2005; Aguilar et al., 2013). Since basal expression of GILZ mRNA shows a circadian pattern in vivo, transcriptional enhancement of GILZ by exogenous CS must be interpreted within this context. As shown in Fig. 8, the response of GILZ to MPL dosing clearly exceeded normal circadian variation in all tissues. Up-regulation of GILZ mRNA was observed as early as 15 minutes after dosing and continued to rise to peak values as late as 8 hours, when plasma MPL concentrations continued to decline. GILZ mRNA eventually re-established its circadian rhythm in all tissues following perturbation by MPL.
estimated parameters for GILZ dynamics (eqs. 10–12) for all three tissues are provided in Table 3.

Fig. 8 shows that GILZ mRNA is upregulated in muscle, but to a lesser extent compared with lung and adipose. GILZ expression is enhanced 0.5 hours after MPL dosing and sharply rises to its peak (15,851 ± 2598 molecules/ng RNA) by 5–6 hours, which was earlier than peak times of GILZ in adipose tissue and lung. Conversely, the peak time of basal mRNA expression in muscle was delayed compared with that in adipose tissue and lung (Fig. 7). In general, the model adequately captured the magnitude of up-regulation of GILZ by MPL as well as its return to circadian baseline, but it overestimated the time of peak response in muscle. This is likely due to the simultaneous fitting of the baseline profile along with the treatment dynamics, where an appreciable difference in times of peak expression was observed. The estimated kd,GILZm in muscle was 0.16 hour⁻¹ (14.3 CV%). The linear stimulatory constant of GILZ mRNA synthesis (SGILZm) in muscle was estimated as 0.27 nM⁻¹ (40 CV%). GILZ mRNA expression was strongly upregulated upon dosing with MPL in adipose, showing a steady increase in expression starting as early as 30 minutes after MPL and reaching its maximum around 8 hours (55,053 ± 1342 molecules/ng RNA), which was well described by the model. The estimated degradation constant of GILZ mRNA (kd,GILZm) in adipose tissue was 0.21 hour⁻¹ (5.8 CV%), which corresponds to a turnover half-life of approximately 3.3 hours. The estimated kd,GILZl lung mRNA was 0.45 hour⁻¹ (7.7 CV%) indicated that the turnover half-life of GILZ mRNA is approximately 1.5 hours in lung, about twice as rapid compared with adipose tissue. The SGILZm in lung was estimated to be 0.47 nM⁻¹ (6.8 CV%). Of interest, although the baseline oscillation of GILZ in lung was more robust than in adipose, the extent of MPL-mediated enhancement of GILZ mRNA from baseline in lung was lower.

**GILZ mRNA Dynamics upon Chronic MPL Dosing.**

The dynamic behavior of steroid-regulated genes can differ based upon the nature of the perturbation introduced within the system (Almon et al., 2007a). The time course of GILZ mRNA expression was assessed in lung and adipose following an infusion of 0.3 mg/kg/h MPL over 7 days. The concentration-time profile for the chronic infusion was simulated based on the parameters in Table 1. The developed pharmacodynamic model was simulated using parameter values obtained for receptor and GILZ dynamics from Tables 2 and 3 to predict GILZ mRNA dynamics in lung and adipose tissue measured from these animals. Chronically elevated steroid concentrations disrupt or even abrogate the circadian rhythmicity of endogenous CST tissue. The SGILZm in lung was estimated to be 0.47 nM⁻¹ (6.8 CV%). Of interest, although the baseline oscillation of GILZ in lung was more robust than in adipose, the extent of MPL-mediated enhancement of GILZ mRNA from baseline in lung was lower.

**TABLE 2**

Parameter values for GR mRNA expression and receptor dynamics

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Definition</th>
<th>Estimate (CV%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>αGRm</td>
<td>Fourier coefficient for GR mRNA</td>
<td>2524/1055.9/2216&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>αGRb</td>
<td>Fourier coefficient for GR mRNA</td>
<td>6.8/162.2/273.2&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>αGRd</td>
<td>Fourier coefficient for GR mRNA</td>
<td>15.6&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>βGR</td>
<td>Fourier coefficient for GR mRNA</td>
<td>0.16&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;d&lt;/sub&gt;GR (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Degradation rate constant for GR mRNA</td>
<td>0.96&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;G&lt;/sub&gt; (nM/h/mol/ng&lt;sup&gt;e&lt;/sup&gt;)</td>
<td>Synthesis rate constant for receptor</td>
<td>0.00025 (5.3)/0.00121 (34.5)/0.00196&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>hGILZ (nM&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Inhibition of GR mRNA production</td>
<td>15.6&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;d,GILZm&lt;/sub&gt; (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Degradation rate constant for receptor</td>
<td>0.05&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;d,GILZl&lt;/sub&gt; (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Degradation rate constant for receptor</td>
<td>0.05&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;d,GILZa&lt;/sub&gt; (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Degradation rate constant for receptor</td>
<td>0.05&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>f&lt;sub&gt;mpl&lt;/sub&gt;</td>
<td>Unbound fraction of MPL in plasma</td>
<td>0.23&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;nf&lt;/sub&gt; (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>DR&lt;sub&gt;b&lt;/sub&gt; loss rate constant</td>
<td>1.23&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>R&lt;sub&gt;t&lt;/sub&gt;</td>
<td>Fraction recycled</td>
<td>0.93&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>k&lt;sub&gt;f&lt;/sub&gt; (h&lt;sup&gt;–1&lt;/sup&gt;)</td>
<td>Translocation rate constant</td>
<td>58.3&lt;sup&gt;a&lt;/sup&gt;</td>
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<tr>
<td>GR&lt;sub&gt;e&lt;/sub&gt; (mol/ng RNA)</td>
<td>GR mRNA initial concentration (treatment)</td>
<td>4000 (fixed)&lt;sup&gt;f&lt;/sup&gt;/1350 (10.7)/2200&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>DR&lt;sub&gt;0&lt;/sub&gt; (nM)</td>
<td>Free cytosolic receptor initial concentration</td>
<td>19.7 (3.3)/25.7 (34.5)/86.2&lt;sup&gt;a&lt;/sup&gt;</td>
</tr>
<tr>
<td>DR&lt;sub&gt;r&lt;/sub&gt; (0) (nM)</td>
<td>Drug-receptor complex initial concentration</td>
<td>0 (fixed)</td>
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<tr>
<td>DR&lt;sub&gt;a&lt;/sub&gt; (0) (nM)</td>
<td>Nuclear complex initial concentration</td>
<td>0 (fixed)</td>
</tr>
</tbody>
</table>

<sup>a</sup>Lung.

<sup>b</sup>Muscle.

<sup>c</sup>Parameter values fixed from Hazra et al. (2007a).

<sup>d</sup>Adipose tissue.

<sup>e</sup>Parameter values fixed from Sukumaran et al. (2011).
measurements from the acute dosing study, enhancement by MPL in lung was appreciably lower compared with adipose tissue. Expression in lung peaked at $31,692 \pm 6050$ molecules/ng RNA and decreased to a steady-state of approximately 23,000 molecules/ng RNA, which was well captured by the model.

**Simulation of Receptor Dynamics upon Chronic MPL Dosing.** Several hypotheses exist for explaining the changes in steroid-regulated tissue gene expression after acute versus chronic dosing. It is possible that molecular events (receptor translocation, recycling, or chromatin binding) are altered during chronic dosing. Alternatively, signal transduction processes involved in generating the response can be amplified or diminished due to the chronic presence of steroid. Furthermore, secondarily induced alterations in other hormones, such as insulin and glucagon, can influence the expression of responsive genes, such as TAT and PEPCK, upon chronic drug exposure (Holten and Kenney, 1967; Jin et al., 2004). To understand the molecular mechanisms governing the tolerance and tissue-specific GILZ dynamics observed with chronic dosing, we performed simulations of the GR mRNA, free cytosolic receptor ($R$), drug-receptor complex ($DR$), and nuclear drug-receptor complex ($DR_n$) in lung and adipose tissue (Fig. 10).

Whereas a rapid down-regulation of receptor mRNA was observed upon steroid exposure in both tissues, it took up to 24 hours for attainment of steady-state. The model predicted a 50–55% decrease in GR mRNA expression from the controls in adipose tissue, which was similar to that observed in liver from chronically infused male ADX rats (Ramakrishnan et al., 2002b). The extent of down-regulation in lung was lower compared with adipose tissue, consistent with our observations in the acutely dosed animals. Cytosolic receptor density took as long as 48 hours before achieving steady-state concentrations in both tissues. The simulated profile of $DR$ concentrations in the cytosol showed a quick increase followed by a relatively rapid decrease to a lower steady state in both tissues. The concentrations of $DR_n$ present in the nucleus peaked at 3 hours into the infusion, which followed the increase and return of $DR$ complex to its own steady-state, with a slight time delay. The time courses of these simulated GR dynamic profiles are in
general agreement with previous chronic infusion studies assessing liver dynamics of ADX animals (Ramakrishnan et al., 2002a). The concentration of $DR_n$ formation in adipose tissue was about 3- to 4-fold higher than $DR_n$ in lung, which might conceivably explain the increased capacity for GILZ gene enhancement in adipose tissue versus lung.

Discussion

Despite increasing clinical use of targeted biologics for immune-related diseases, CS remain a cornerstone in therapy owing to their widespread immunosuppressive effects. Among a few other transactivated genes, GILZ has been implicated in mediating anti-inflammatory CS effects (Ayroldi and Riccardi, 2009; Vandevyver et al., 2013). In this report, we sought to establish a mechanistic and quantitative basis using PK/PD modeling for the tissue-specific enhancement of GILZ by MPL under different dosing regimens in vivo.

CS exert therapeutic and adverse effects in various organs via a coupled receptor-mediated mechanism. The catabolic effects of MPL dosing on organ weights display different sensitivities or capacities to respond to steroid treatment, which are dependent upon drug-receptor association and receptor densities within the tissues (Ramakrishnan et al., 2002b). Less is known regarding the precise mechanisms controlling differences in expression of a single or multiple genes across tissues. Here, we examined whether such tissue-specific regulation of GR controls differences at the level of gene expression across tissues.

Endogenous glucocorticoid production from the adrenal cortex is regulated in a circadian fashion by the hypothalamic-pituitary-adrenal axis via input from the suprachiasmatic nucleus, consequently producing oscillations in steroid-regulated genes in tissues. Such time-dependent variations in gene expression influence drug action, including pharmacodynamic responses, due to the availability or functioning of target proteins (Sukumaran et al., 2010). Hence, conclusions made from time-course studies require consideration of such oscillatory behaviors. All measures of GR and GILZ mRNA expression examined in our study displayed circadian oscillations. We examined the circadian regulation of GR mRNA and its dynamics after acute MPL dosing in skeletal muscle, lung, and adipose tissue. Although it was not surprising to find that the amount of receptor mRNA expression varied across tissues, it was interesting to identify distinct, tissue-specific patterns of circadian rhythmicity, which can be of physiologic importance. For example, the nadir of GR rhythmicity in skeletal muscle occurred at the transition from light to dark, which coincides with the time of peak plasma CST concentration. This pattern is in direct contrast to adipose tissue, where GR mRNA peaked at the light-to-dark transition period. Such divergent tissue behavior may be explained from the standpoint of energy metabolism (Laposky et al., 2008). Since the animal is not feeding during the light/inactive period, it is dependent upon free fatty acid release from lipolysis as its main energy source, explaining a timely increase in GR expression to facilitate this process in adipose. Conversely, since glucocorticoids promote net protein degradation in muscle (Vegiopoulos and Herzig, 2007), decreased GR expression might serve as a protective mechanism against this effect. The circadian pattern of GR in lung was entrained to

![Fig. 9. GILZ mRNA expression in lung and adipose tissue from rats infused with 0.3 mg/kg/h SC MPL for 7 days. Solid circles represent experimental data from individual rats, and solid lines are simulations using the PK/PD model depicted in Fig. 3. The parameters used are those for acute steroid effects listed in Table 3.](image-url)
adrenal CST production, but the direct physiologic relevance of this behavior is not apparent. The MPL bolus dosing led to a rapid decrease in receptor mRNA in all three tissues, consistent with previous findings of tissue-specific GR mRNA regulation by dexamethasone (Kalinyak et al., 1987). The tissue dynamics followed relatively similar patterns over time, likely due to similar degradation-rate constants.

The GILZ mRNA regulation in all three tissues followed a pattern that is entrained to the CST rhythm. CST, however, only partially controls the cyclic GILZ expression, since adrenalectomy does not completely abolish the circadian rhythm of GILZ mRNA in tissues (Sotak et al., 2016). Our results provide in vivo confirmation of prior in vitro studies (D’Adamio et al., 1997; Smit et al., 2005; Aguilar et al., 2013), showing that GILZ transcription is strongly enhanced upon CS exposure. The half-life of GILZ mRNA expression was estimated to be around 3–4 hours in muscle ($k_{d,GILZm} = 0.16$ hour$^{-1}$) and adipose tissue ($k_{d,GILZm} = 0.21$ hour$^{-1}$) and 1.5 hours in lung ($k_{d,GILZm} = 0.45$ hour$^{-1}$). Differences in mRNA degradation rate could arise from cell- or tissue-specific differences in cytoplasmic mRNA decay mechanisms (Linde et al., 2007; Schoenberg and Maquat, 2012). The concerted regulation of circadian rhythmicity and CS pharmacodynamics was apparent in lung and adipose tissue based upon simultaneous model fitting of the circadian and acute dosing profiles. The dynamics of GILZ in muscle, however, showed some divergence in the circadian and treatment profiles, which led to a discrepancy between the observed and model-estimated times of peak response in the treatment group. This could be caused by the direct tissue-specific effects of CS, which produce an apparent phase shift in peripheral-clock response in intact animals (Balsalobre et al., 2000), which was not accounted for in this model. While we speculate that the higher sensitivity constant ($S_{GRILZ}^{DE}$) in lung (beyond receptor differences) may arise due to the distinct primary roles of CS in lung versus muscle and adipose (i.e., immune versus metabolic regulation), our findings based on in vivo measurements may provide some basis for further experimental assessments of this molecular process in vitro.

Chronic MPL produced a different dynamic behavior of GILZ expression compared with acute dosing. Prior microarray studies in muscle and liver following chronic MPL infusion indicated that various temporal patterns emerge for the drug-regulated genes (Almon et al., 2007a,b). GILZ dynamics in both lung and adipose tissue showed a recognizable pattern where expression was rapidly enhanced to a peak, but then decreased over 24 hours to achieve a new steady-state that was maintained until the end of the 7-day study period.

Quantitative systems modeling was used to understand the dynamic mechanisms controlling tissue-specific MPL effects. Assuming the kinetics of drug entry into the tissues studied are not rate-limiting (i.e., well perfused tissue entry), the dissociation constant for the drug-receptor binding and the free receptor density (as controlled by de novo receptor synthesis and degradation, the recycled fraction, and receptor mRNA autoregulation) would limit the overall response of tissues to steroid treatment. We therefore measured the dynamics of GR message expression in the selected tissues and simulated tissue-specific free receptor densities using our

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**Fig. 10.** Simulated profiles of the driving forces (GR mRNA, free cytosolic receptor, and drug-receptor complex in the cytosol and nucleus) controlling GILZ regulation in lung and adipose tissue from rats infused with 0.3 mg/kg/h MPL for 7 days. Simulations are based on the model in Fig. 3. The parameters are those for acute MPL effects as listed in Tables 2 and 3.
model. The short half-life of MPL (~30 minutes) resulted in steady-state concentrations being achieved within a few hours during chronic infusion. However, simulation of lung and adipose tissue receptor dynamics showed that it takes at least 24 hours for the steady-state to be attained, consistent with the time course of receptor measures in ADX liver (Ramakrishnan et al., 2002b). The fifth-generation model captured GILZ dynamics in both tissues while demonstrating that receptor down-regulation was the common mechanism controlling the tolerance in pharmacogenic responses. Also demonstrated was that tissue-specific concentrations of the steroid-receptor complex (DRx) corresponded with the capacity of MPL-mediated GILZ enhancement in those tissues. Interestingly, the same model indicated that post-receptor events contributed to a decoupling between receptor dynamics and hepatic TAT gene induction during long-term dosing, attributed to secondarily induced changes in insulin, which also regulates TAT (Ramakrishnan et al., 2002b). Our model simulations suggest that certain parameters such as \( k_{on}, k_{off}, k_t, \) and \( R_f \) fixed to constant values across the tissues based on bolus dose estimates, are less likely to influence the divergence in the tissue- and dosage regimen-dependent behaviors of GILZ in vivo.

A salient feature of this study is that replicate data obtained from both circadian and MPL experiments were modeled jointly to obtain parameter values. Despite the model being developed based on a single dose and using a linear stimulation coefficient (SSILZ) instead of a more appropriate saturable effect function, the final model well predicted GILZ dynamics upon chronic steroid exposure. A limitation is the assumption of a normal CST rhythm in acutely dosed animals. In reality, MPL causes suppression of endogenous CST by binding to GR in the pituitary, thereby modulating its release from the adrenal cortex (Cole et al., 2000; Yao et al., 2008). This, in turn, could modulate endogenous GILZ expression. However, MPL binds GR with higher affinity than CST, predominantly exerting receptor/gene-mediated effects when present in the system. Furthermore, adrenalectomy dampens the amplitude but does not abolish circadian GILZ expression in tissues (Sotak et al., 2016), possibly indicating an added regulatory mechanism involving peripheral clock genes. Since inclusion of these processes without additional data would have resulted in overparameterization, a semimechanistic IDR approach based on Fourier harmonics was used to describe the nonstationary circadian rhythms, providing a physiologically integrated and genomics on the molecular and tissue levels while accounting in baselines.

An important class of therapeutic agents. These studies quantitatively assess CS kinetics, dynamics, and genomics on the molecular and tissue levels while accounting for circadian rhythms, providing a physiologically integrated and genomics on the molecular and tissue levels while accounting in baselines.


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