

Intracellular Delivery of the P38 MAPK Inhibitor SB202190 in Renal Tubular Cells: a Novel Strategy to Treat Renal Fibrosis

Jai Prakash, Maria Sandovici, Vinay Saluja, Marie Lacombe, Roel Q.J. Schaapveld, Martin de Borst, Harry van Goor, Robert H. Henning, Johannes H. Proost, Frits Moolenaar, Gyorgy Keri, Dirk K.F. Meijer, Klaas Poelstra, Robbert J. Kok

Department of Pharmacokinetics and Drug Delivery (J.P., V.S., J.H.P., F.M., D.K.F.M, K.P., R.J.K.), Department of Clinical Pharmacology (M.S., R.H.H.) and Department of Pathology and Laboratory Medicine (M.D.B., H.V.G.) Groningen University Institute for Drug Exploration (GUIDE), Groningen, The Netherlands.

Kreatech Biotechnology B.V., Vlierweg 20, 1032 LG Amsterdam, The Netherlands. (M.L., R.Q.J.S.).

Vichem Chemie Research Ltd., Budapest, Hungary. (G.K.)

Department of Pharmaceutics, Utrecht University, The Netherlands. (R.J.K.)

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Corresponding Author:

Jai Prakash

Department of Pharmacokinetics and Drug Delivery

Groningen University Institute for Drug Exploration

Antonius Deusinglaan 1

9713 AV, Groningen

The Netherlands

Email: J.Prakash@rug.nl

Tel: +31-50-3633281

Fax: +31-50-3633247

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expressed and secreted; HPLC, high performance liquid chromatography, FCS, fetal calf

serum; ESI-MS, electronspray ionization mass spectrometry; PBS, phosphate buffered saline;

GSH, glutathione

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Abstract

During renal injury, activation of p38 MAPkinase in proximal tubular cells plays an important role in the inflammatory events that eventually lead to renal fibrosis. We hypothesized that local inhibition of p38 within these cells may be an interesting approach for the treatment of renal fibrosis. To effectuate this, we developed a renal specific conjugate of the p38 inhibitor SB202190 and the carrier lysozyme. First, we demonstrated that SB202190 inhibited the expression of albumin-induced proinflammatory (MCP-1) and TGFβ1-induced profibrotic (procollagen-Iα1) genes over 50% in renal tubular cells (NRK-52E). Next, we conjugated SB202190 via a carbamate linkage to lysozyme. However, this conjugate rapidly released the drug upon incubation in serum. We therefore applied a new platinum(II) based linker approach, so-called Universal Linkage System (ULSTM), which forms a coordinative bond with SB202190. SB202190-ULS-lysozyme remained stable in serum but released the drug in kidney homogenates. SB202190-ULS-lysozyme accumulated efficiently in renal tubular cells and provided a local drug reservoir during a period of 3 days after a single i.v. injection. Treatment with SB202190-ULS-lysozyme inhibited TGF-β1induced gene expression for procollagen-Iα1 by 64% in HK-2 cells. Lastly, we evaluated the efficacy of a single dose of the conjugate in the unilateral renal ischemia-reperfusion rat model. A reduction of intrarenal p38 phosphorylation and alpha-smooth muscle actin protein expression was observed 4 days after the ischemia-reperfusion injury. In conclusion, we have developed a novel strategy for local delivery of the p38 MAPkinase inhibitor SB202190 which may be of use in the treatment of renal fibrosis.

Introduction

Efficient treatment of renal fibrosis is one of the major challenges in the field of nephrology as there is a trend of a continuously increasing number of patients each year world wide (Meguid El and Bello, 2005). Current therapies such as inhibition of reninangiotensin system components have yet not been able to prevent end-stage renal diseases, and therefore more specific approaches are required. It has been described that renal tubular cells play a pivotal role in the initiation of inflammatory processes leading to interstitial fibrosis (Strutz, 2001). During a renal insult, tubular cells are activated by various stimuli such as filtered proteins, cytokines or hypoxia, upon which they produce several proinflammatory chemotactic factors (MCP-1 and RANTES) and profibrotic factors (TGFβ1) (Takaya et al., 2003; Zoja et al., 1998; Morigi et al., 2002; Wolf et al., 2004). These factors further activate tubular cells, macrophages and fibroblasts. P38 mitogen-activated protein kinase (MAPK) plays a crucial role in the activation of tubular cells and in the secretion of various cytokines from tubular cells (de Borst et al., 2005). Therefore, blockade of p38 in tubular cells may be valuable for the treatment of renal injuries. The beneficial role of p38 inhibitors has been demonstrated for the treatment of renal injuries (Koshikawa et al., 2005; Stambe et al., 2004). However, tubular cell-specific effects were not delineated and relatively high doses were required to achieve a therapeutic effect. Moreover, several clinical trials showed that p38 inhibitors exerted various side effects in other organs, such as immunosuppression, as reviewed (Kumar et al., 2003). Such a systemic immunosuppressive effect of a drug against renal fibrosis is unfavorable. We therefore hypothesized that renal specific drug delivery can greatly improve the therapeutic profile of p38 MAPkinase inhibitors for renal disorders.

Target-cell specific drug delivery is an attractive approach to investigate the cellspecific effects of drugs, as it can avoid interactions with non-targeted cells in other organs

and thereby decrease side-effects. Furthermore, drug delivery can augment local drugs levels at the target site, thereby improving therapeutic efficacy. We have gathered unique expertise in delivering the drugs to the kidneys using the low molecular weight protein lysozyme (LZM) as drug carrier (Haas et al., 2002). We now propose to utilize drug-LZM conjugates for the delivery of antifibrotic kinase inhibitors. Recently, we evaluated the pharmacokinetics of the well-known p38 inhibitor SB202190 (4-(4-Fluorophenyl)-2-(4-hydroxyphenyl)-5-(4-pyridyl)1H-imidazole) and demonstrated that it distributed poorly to the kidneys (Prakash et al., 2005b). This result underscored the need for drug delivery of this type of hydrophobic compounds to achieve appropriate drug levels in the kidney, which predominantly accumulates hydrophilic compounds.

Although SB202190 has been used extensively as model compound for p38 inhibition, only a few studies report its use in renal tubular cells, e.g. after activating them with angiotensin II and insulin (Bhaskaran et al., 2003; Harrison et al., 2006). In these studies, SB202190 reduced angiotensin II-induced apoptosis in tubular cells but did not alter the effect of insulin in these cells. In the present study, we therefore first evaluated the effect of SB202190 on fibrotic signaling cascades in renal tubular cells. Furthermore, we conjugated SB202190 to LZM via two different strategies: we conjugated the drug via a carbamate linkage which appeared suitable for the hydroxyl group of SB202190 and we employed a new platinum-based linkage system called Universal Linkage System (ULSTM) to couple the drug via a coordinative bond at its pyridinyl group. The latter coupling strategy offers advantages with respect to the synthesis and stability of the constructs. Since platinum compounds are known to produce nephrotoxicity (Park et al., 2002; Wolfgang et al., 1994), we investigated the SB202190-ULS-LZM conjugate (further referred to as SB-ULS-LZM) for cytotoxicity in renal tubular cells in cell cultures and *in vivo*. In addition, we investigated the drug release profile of the SB-LZM conjugates *in vitro* and evaluated the

pharmacokinetics of SB-ULS-LZM in normal rats. Lastly, we tested the capability of SB-ULS-LZM to interfere with fibrotic signaling events in human renal tubular cells *in vitro* and in the unilateral ischemia-reperfusion renal injury model *in vivo* in rats.

Materials and Methods

Cells and Animals

NRK-52E (normal rat kidney) cells were kindly provided by Prof. Russel, University of Nijmegen, The Netherlands. Cells were cultured in DMEM medium (BioWhittaker, Verviers, Belgium) supplemented with 5% fetal calf serum (FCS, BioWhittaker), 4 mM L-glutamine, penicillin (50 units/ml) and streptomycin (50 ng/ml). Human kidney tubular cells (HK-2) were obtained from ATCC (Manassas, VA) and grown in RPMI-1640 medium supplemented with 10% FCS, 2 mM L-glutamine, penicillin (100 units/ml) and streptomycin (100 ng/ml). Human recombinant TGF-β1 was purchased from Roche Diagnostics, Mannheim, Germany.

All experimental protocols for animal studies were approved by the Animal Ethics Committee of the University of Groningen. Normal male Wistar rats (220-240 g) were obtained from Harlan (Zeist, The Netherlands).

Determination of mRNA expression

After the treatments (as described in the legends of the figures), cells were harvested using lysis buffer and total RNA was isolated from the cells using Stratagene Microkit (Stratagene, La Jolla, CA). RNA content was measured by a nanodrop UV-detector (NanoDrop Technologies, Wilmington, DE). cDNA was synthesized from the similar amount of RNA using the Superscript III first strand synthesis kit (Invitrogen, Carlsbad, CA). Gene expression levels for the following genes were measured by quantitative real-time RT-PCR (Applied Biosystems., Foster City, CA). The primers for rat species were obtained from Sigma-Genosys (Haverhill, UK) as follows: monocyte chemoattractant protein-1 (MCP-1; 5'-TCCTCCACCACTATGCAGGT-3' and 5'-TTCCTTATTGGGGTCAGCAC-3', 255 bp), tissue inhibitor of metalloproteinase-1 (TIMP-1; 5'-GAGAGCCTCTGTGGATATGT-3' and

5'-CAGCCAGCACTATAGGTCTT-3', 334 bp), procollagen-Iα1 (5'-AGCCTGAGCCAGCAGATTGA-3' and 5'-CCAGGTTGCAGCCTTGGTTA-3', 145 bp) and glyceraldehyde-3-phosphate dehydrogenase (GAPDH; 5'-CGCTGGTGCTGAGTATGTCG-3' and 5'-CTGTGGTCATGAGCCCTTCC-3', 179 bp). The Taqman primers for Human species were obtained from Applied Biosystems (Assay–On–Demand).

For NRK-52E cells, SYBR® Green PCR Master Mix (Applied Biosystems, Warrington, UK) was used as a fluorescent probe for real-time RT-PCR. For each sample, 1 μl of cDNA was mixed with 0.4 μl of each gene-specific primer (50 μM), 0.8 μl DMSO, 8.4 μl water and 10 μl SYBR Green PCR Master Mix. For HK-2 cells, qPCRTM Mastermix Plus (Eurogentec, Seraing, Belgium) was used as a fluorescent probe for real-time RT-PCR. For each sample, 1.25 μl of cDNA was mixed with 0.5 μl of each gene-specific primer, 4.5 μl water and 5 μl qPCRTM Mastermix Plus. The cDNA amplification was performed until 40 cycles. Finally, the threshold cycle number (Ct) was calculated for each gene and relative gene expressions were calculated after normalizing for the expression of the control gene GAPDH.

Synthesis of SB-carbamate-LZM

The synthesis strategy is outlined in **Fig. 2A**. SB201290 (3 µmol, L.C. Laboratories, Woburn, MA)) was reacted with N-succinimidyl-N-boc-ethylenediamine (NSED, 90 µmol, Sigma, St. Louis, MO) in dichloromethane in the presence of tributylamine (60 µmol) with stirring for 24 hours at room temperature. After completion of the reaction, as demonstrated by thin layer chromatography (silica plates, ethylacetate: acetone, 1:1 v/v) the intermediate product was purified on preparative silica TLC and characterized by electronspray ionization mass spectrometry (ESI-MS) and HPLC analysis. The boc–group was removed by incubating

with 10 % trifluoroacetic acid for 1 h. Following evaporation of the acid under reduced pressure, the deprotected amine (3 µmol) was then reacted with γ-maleimidobutyryloxysuccinimide ester (GMBS, 2.7 μmol, Sigma) in dimethylformamide (DMF) and dichloromethane (1:1) for 1 h in the presence of tributylamine (42 µmol). The product was evaluated by ESI-MS and HPLC analysis. Total amount of SB202190-carbamate product was calculated by estimating SB202190 with HPLC analysis by detaching it in strong basic condition.

To introduce thiol groups that can be reacted with the maleimidyl group of the SB202190-carbamate adduct, egg-white LZM (1.4 μmol, Sigma) was modified with N-Succinimidyl-S-acetylthioacetate (2.1 μmol, Sigma) in 0.1 M PBS for 1 h. The product was dialysed against phosphate buffered saline (PBS, pH 7.4) for 24 h and the purified product was treated with 0.1 M hydroxylamine and ethylenediaminetetraacetic acid mixture to deprotect the thiol group. The SB202190-carbamate product (2.8 μmol) dissolved in DMF was slowly added to the solution of LZM–SH (1.4 μmol) in PBS (pH 7.4) and reacted for 2 hours at room temperature. The final product was dialyzed against water, filtered with 0.2 μm syringe filter, lyophilized and stored at -20°C. The conjugate was characterized by ESI-MS analysis for the whole conjugate and by HPLC analysis for SB202190, as described earlier (Prakash et al., 2005b). For this latter analysis, the coupled drug was released by incubating with 0.5 M NaOH at 37°C for 24 h.

Synthesis of SB-ULS-LZM

Synthesis of SB202190-ULS

The synthesis strategy is outlined in **Fig. 2B**. SB202190 was coupled with ULS in 1:1 molar ratio. Cis-[Pt(ethylenediamine)nitrate-chloride] (ULS; 5.2 µmol) was added to SB202190 (5.4 µmol, 10 mg/ml in DMF) and heated at 37°C for 3 h. The reaction mixture

then was evaporated to dryness under reduced pressure, affording a pale yellow solid (yield 92%) that was analyzed by HPLC, ¹HNMR and ESI-MS, These analyses confirmed the 1:1 coupling ratio of drug and linker.

¹H NMR of free **SB202190** (CD₃OD): $\delta_{\rm H}$ 6.88 (d, J = 8.74 Hz, 2H, F(CHC**H**)₂), 7.17 (m, 2H, N(CHC**H**)₂), 7.50 (m, 4H, (C**HCH**)₂OH), 7.82 (d, J = 8.68 Hz, 2H, F(CHC**H**)₂), 8.41 (m, 2H, N(CHC**H**)₂) ppm.

¹H NMR of **SB202190**-[Pt(ethylenediamine)dichloride] (CD₃OD): $\delta_{\rm H}$ 2.59 (m, 4H, H₂N(C**H**₂)₂NH₂), 5.58 (s, 2H, NH₂), 5.91 (s, 2H, NH₂), 6.89 (d, J = 8.75 Hz, 2H, F(CHC**H**)₂), 7.22 (m, 2H, N(CHC**H**)₂), 7.53 (m, 4H, (C**HCH**)₂OH), 7.82 (d, J = 8.73 Hz, 2H, F(CHC**H**)₂), 8.52 (m, 2H, N(CHC**H**)₂) ppm.

MS (ESI⁺) m/z: 622 [M+H]⁺, 585 [M-Cl⁻-H⁺]⁺.

Synthesis of SB-ULS-LZM

Drug-ULS adducts react readily with thiol groups of methionine and cysteine residues at 37°C, as has been demonstrated with albumin carrier proteins (Gonzalo et al., 2006). Pilot experiment showed that LZM did not react readily with fluorescein-ULS (data not shown), presumably because the methionine residues and disulfide bridges are buried in the core of the protein. We therefore introduced additional methionine residues onto the protein surface by chemical derivatization of lysyl residues. Boc-L-methionine hydroxysuccinimide ester (0.84 μmol, Fluka, Germany) was dissolved in dimethyl sulfoxide and added to LZM (0.7 μmol, 10 mg/ml in 0.1 M sodium bicarbonate buffer, pH 8.5). The mixture was stirred for 1 h at room temperature. The product was dialyzed against water for 48 h, filtered through 0.2-μm membrane filter, lyophilized and characterized by ESI-MS analysis. Methionine-LZM was further reacted with SB202190-ULS to obtain the final SB-ULS-LZM conjugate. SB202190-ULS (2.1 μmol) in DMF was added to methionine-LZM (0.7 μmol) dissolved in

ULS labeling buffer (20 mM tricine/NaNO₃ buffer pH 8.5). The mixture was reacted at 37°C for 24 h, after which the product was dialyzed against water for 48 h, filtered, lyophilized and stored at -20°C. ESI-MS and HPLC analysis of the coupled SB202190 were performed to confirm the composition of the SB-ULS-LZM conjugate. The conjugated drug was determined after releasing the drug from the SB-ULS-LZM conjugate by competitive displacement with an excess of thiocyanate, which is an excellent ligand for platinum-coordination. In brief, appropriate aliquots of the conjugate (0.2 mg/ml in PBS) were incubated with 0.5 M potassium thiocyanate in PBS at 80°C for 24. The released SB202190 was estimated by HPLC as described before (Prakash et al., 2005b). Free drug levels in the preparation were also investigated by HPLC analysis of freshly prepared appropriate dilutions of the conjugate in PBS.

Stability of the conjugates

Drug-free serum and kidneys were obtained from healthy male Wistar rats. Kidney homogenates were prepared in PBS (pH 7.4) or sodium acetate buffer (pH 5.0) in 1:3 w/v using an Ultra-Turrax-T25 apparatus (IKA, Stauffen, Germany) at the highest speed. All matrices were kept on ice before incubation with the conjugate. SB-carbamate-LZM was incubated with PBS, serum and kidney homogenates (pH 7.4 and pH 5.0) whereas SB-ULS-LZM was incubated in the conditions listed above and in 0.1 M sodium acetate buffer (pH 5.0), 5mM glutathione (GSH) in PBS, and kidney homogenates at pH 7.4 and pH 5.0. Incubations were performed at 37°C and 100 μl aliquots were taken at 2, 6 and 24 h, after which they were processed immediately for HPLC analysis of SB202190.

Assessment of the toxicity of ULS conjugates

We determined the platinum-related cellular toxicity of the SB-ULS adduct and its

lysozyme conjugate in the renal tubular cell line NRK-52E. Cells were seeded at 10^4 cells/well in 96-well plates in culture medium (200 μ l). After 24 h of incubation, medium was replaced by medium containing different dilutions of cisplatin or the ULS-containing compounds. Plates were incubated for 24 h, after which cell viability was assessed by Alamar Blue assay (Serotec, Oxford, UK).

Pharmacokinetics of SB-ULS-LZM

Rats (n=11) were injected with a single dose of the SB-ULS-LZM conjugate (16 mg/kg equivalent to 376 µg/kg of SB202190, dissolved in 5% glucose) that was administered intravenously through the penile vein under inhalation anesthesia. Animals were placed back into metabolic cages to collect urine, which was combined with urine collected from the urinary bladder after sacrificing the animals. At each indicated time point except 24 h (n=2), a single animal was sacrificed. This procedure was chosen to characterize the pharmacokinetics of the compounds, allowing multicompartmental curve-fitting (see below). At 5, 15 min, and 1, 2, 6, 12, 24, 36, 48 and 72 h, animals were anesthetized and blood samples were collected by heart puncture and kidneys were isolated after gently flushing the organs with saline. Kidneys were weighed and half of the kidney was homogenized (1:3 w/v, PBS) which was stored at -80°C. Released drug amounts were estimated by HPLC analysis after extraction as described above. To estimate total drug (bound plus released), samples were treated with potassium thiocyanate to release SB202190 from the ULS linker as described above and then subjected to HPLC analysis. Anti-LZM immunohistochemical staining was performed on frozen kidney sections to detect the renal uptake of the conjugate.

In vivo toxicity of ULS after administration of SB-ULS-LZM was assessed in the same animals as used for the pharmacokinetic study, and compared to untreated animals (n=4) and to the animals treated with a dose of cisplatin (3 mg/kg, i.v., n=4) for 24 h. This

dose of cisplatin is 8-fold higher than the amount of platinum in the SB-ULS-LZM conjugate. To examine the effect on the renal function, serum and urine creatinine levels were determined to calculate creatinine clearance. In case of SB-ULS-LZM treated animals, creatinine clearance at 24, 32, 48 and 72 h was calculated from serum and urine samples collected at the latest 24 h before sacrificing the animals. To calculate proteinuria for the SB-ULS-LZM group, the mean of the urinary protein levels at different days was taken. TUNEL staining and Masson staining were performed on kidney cryostat sections to examine the number of apoptotic cells and changes in renal morphology. In addition, we determined the platinum levels in kidneys using Inductively Coupled Plasma–Atomic Absorption Spectrometry (ICP-AAS) after digestion of the tissue in concentrated nitric acid for 24 h at room temperature and heating at 70°C until the formation of clear solution.

Efficacy of SB-ULS-LZM in unilateral ischemia-reperfusion (I/R) rats

The pharmacological efficacy of SB-ULS-LZM was evaluated in the unilateral ischemia-reperfusion (I/R) rat model. At 2 h prior to the ischemia procedure, rats were injected with SB-ULS-LZM (32 mg/kg of conjugate, equivalent to 752 μg/kg SB202190; n=6), vehicle (5% glucose; n=6), or free SB202190 (800 μg/kg; n=3). SB-ULS-LZM was dissolved in 5 % glucose whereas SB202190 was dissolved in 20 % hydroxypropyl-β-cyclodextrin solution with 5 % DMSO as described earlier (Prakash et al., 2005b). Compounds were administered intravenously via the penis vein as described above. Animals were allowed to recover and placed back into the cages until the induction of renal ischemia. Rats were operated and the renal artery and vein were clamped under microscope to stop renal blood flow. After 45 min, clamps were removed and reperfusion of the kidney was observed before closing of the wound. Sham-operated animals (n=3) received the same surgical procedure except ischemia, were included as a control group. After 4 days, animals were sacrificed and blood samples

were collected from the abdominal aorta. Kidneys were isolated after gently flushing the organs with saline and preserved in 4 % formalin for preparation of paraffin–embedded sections, or frozen in icecold isopentane for preparation of cryosections.

Histological and Immunohistochemical analyses

Kidney cryostat sections were used for immunohistochemical detection of LZM, α-SMA, TUNEL positive cells and for Masson staining. Cryostat sections of 4-μm thickness were fixed with acetone and incubated with rabbit anti-LZM polyclonal IgG (dilution 1:500, Chemicon, Temecula, CA) or anti-α-SMA monoclonal IgG (dilution 1:500, Sigma) for 1 h at room temperature. After washing with PBS, sections were incubated with hydrogen peroxide (0.07 % in PBS) to inactivate endogenous peroxidase activity and subsequently incubated with goat anti-rabbit or rabbit anti-mouse horseradish peroxide conjugated antibodies (dilution 1:50, Dako, Denmark) for 20 min. Peroxidase activity was visualized with 3-amino-9-ethylcarbazole as red color. Sections were counter-stained with hematoxylin and mounted with Kaiser's glycerin gelatin solution. TUNEL staining (TUNEL Pod Kit, Roche Diagnostics) was performed according to the supplier's protocol. Positively stained cells were counted in 10 different fields (magnification, 200×) of kidney cortex region using NIH Image J software. Masson staining was performed according to standard protocols.

Anti-p-p38 immunohistochemical staining was performed on 3-µm thick paraffin—embedded sections. Sections were deparaffinized in xylene and rehydrated in alcohol and distilled water. To retrieve antigen, sections were boiled in 10 mM citrate buffer pH 6.0 for 10 min in microwave and cooled down. Then, sections were incubated with 3 % hydrogen peroxide for 10 min. After washing in distilled water, sections were blocked with 1% BSA for 1 h and incubated with rabbit anti-p-p38 monoclonal IgG (Dilution 1:100, Cell signaling, Danvers, MA) overnight at 4°C. After washing 3 times with Tris—buffered saline

(pH 7.6), section were incubated with secondary goat-anti-rabbit antibody and subsequently with rabbit-anti-goat hydrogen peroxidase, Dako, Denmark, each for 20 min. Finally, staining was developed with 3,3'diaminobenzidine tetrahydrochloride (DAB).

Semi-quantification of α -SMA and p-p38 immunohistochemical staining was performed by two independent observer in a double-blind manner. Each section was scored as following: –, negative; –/+, faint staining; +, occasional positive; ++, strong; +++, abundant staining.

Statistical analysis

The statistical analyses were performed using Student's t-test with p<0.05 as the minimal level of significance. Results are presented as mean \pm standard error of the mean. Pharmacokinetic analysis of the plasma SB202190 concentrations was performed using the Multifit program (Department of Pharmacokinetics and Drug Delivery, University of Groningen, The Netherlands).

Results

Effect of SB202190 on fibrotic signaling in renal tubular cells

To investigate the effect of SB202190 on pro-inflammatory and pro-fibrotic signaling cascades in renal tubular cells, we activated NRK-52E cells with either bovine serum albumin (BSA, 30 mg/ml) or TGF-β1 (10 ng/ml). Albumin stimulated the gene expression of the inflammation marker MCP-1 over 30-fold, which in turn could be reduced by 55% after p38 inhibition (**Fig. 1A**). Furthermore, BSA enhanced the gene-expressions of TIMP-1 significantly, while procollagen–Iα1 was not elevated significantly (**Fig. 1B-C**). Treatment with SB202190 reduced the expression of these genes to levels below basal expression, as was also observed for non-activated cells that were treated with the drug. Similarly TGF-β1 also induced the gene expression of procollagen–Iα1 and TIMP-1 significantly in 24 h and, treatment with SB202190 inhibited the gene expression of all the genes significantly (**Fig. 1B-C**). MCP-1 expression was not effected by TGF-β1 treatment (data not shown).

Synthesis and characterization of SB202190-LZM conjugates

SB-carbamate-LZM conjugate (Fig. 2A)

SB202190 was converted to SB202190-NSED with an overall yield of 88% after purification, as estimated by HPLC analysis. Next, SB202190-NSED was reacted with GMBS and provided the SB202190-carbamate linker adduct at 90% yield. SB202190-carbamate was reacted to thiol-modified LZM which produced a SB-carbamate-LZM conjugate with an average drug/carrier ratio of 0.7:1, as characterized by mass spectrometry of the whole conjugate and by HPLC analysis of the coupled drug.

SB-ULS-LZM conjugate (Fig. 2B)

SB202190 was efficiently coupled with ULS yielding the drug-ULS 1:1 adduct at an overall yield of 92%. The identity of the product was confirmed by HPLC, ¹HNMR and ESI-

MS. ¹H NMR and Pt-NMR studies indicated that SB202190 was coordinated to ULS at the pyridinyl nitrogen of the drug. The resulting methionine-LZM carrier was straightforwardly converted in the SB-ULS-LZM product by incubating with drug-ULS overnight. The final product was characterized by mass spectrometry of the whole conjugate and by HPLC analysis of the coupled drug, confirming 1:1 drug to protein coupling.

In an ideal drug delivery conjugate, the drug-carrier linkage should be stable during storage and in the systemic circulation in order to reach the target cells intactly. In addition, the linkage should display an appropriate drug-release profile once the conjugate has been accumulated in target cells, to provide the pharmacologically active compound. **Fig. 3A** and **3B** show the drug-release profile of the SB-carbamate-LZM and SB-ULS-LZM conjugates, respectively. A clear difference was observed in the stability of the two types of conjugates. SB-carbamate-LZM was unstable in PBS and even more unstable in serum whereas SB-ULS-LZM conjugate remained stable in both media. In kidney homogenate, the target tissue of the constructs, both conjugates displayed gradual release of the drug at pH 7.4, but at pH 5.0 only SB-ULS-LZM did release the drug (**Fig. 3A and 3B**). Since the constructs are taken up via endocytosis and drug release should occur in lysosomes (pH 5.0) this is quite relevant. In vivo, endogenous compounds such as GSH can bind to platinum and thereby displace the drug. We found that SB-ULS-LZM released the drug maximally at 2 h after incubating with GSH and no further release occurred until 24 h. Based on the release profile in serum and kidney homogenates, we decided to pursue our study with SB-ULS-LZM.

Toxicity of platinum containing compounds in tubular cells

The effect of ULS on viability of renal tubular epithelial cells (NRK-52E) was compared with an equimolar concentration of the well-known cytostatic drug cisplatin. ULS showed no effect on the viability of the cells at the concentration of $100~\mu M$, whereas

cisplatin caused a significant reduction of the number of viable cells (**Fig. 4A**). We also tested the drug-ULS and drug-ULS-LZM constructs and found them non-toxic in comparison to their respective controls (**Fig. 4B and 4C**).

Pharmacokinetics of SB-ULS-LZM conjugate

In prior studies with other drug-LZM conjugates, we observed a rapid renal accumulation of these products after intravenous administration (Prakash et al., 2005a). We used this knowledge to design a protocol for the pharmacokinetic studies with SB-ULS-LZM that allowed optimal estimation of the pharmacokinetic parameters. In such a so-called optimal sampling protocol, the data are fitted to a non-linear multi-compartment model (Multifit program). The serum-disappearance curve of SB-ULS-LZM, which followed a twocompartment pharmacokinetic model, is shown in Fig. 5. Since we sacrificed the individual animals at different time points rather than at fixed moments in time, calculated parameters are less prone to extrapolation and are consequently more reliable (Table 1). Only carrier-bound SB202190 was detected in the serum, while free drug was absent at all time points. From this result, we concluded that the conjugate remained stable in the serum. Furthermore, in accordance to other drug-LZM conjugates, SB-ULS-LZM accumulated efficiently in the kidneys within 1 h following the intravenous injection (Fig. 6A). The accumulation of the conjugate in proximal tubular cells was confirmed by anti-LZM immunohistochemical staining on kidney sections (Fig. 6C-D). In parallel with the accumulation of ULS-bound drug, we observed continuous levels of free SB202190 in the kidneys at all time points starting from 1 h after dosing until the last sampling point, 3 days after injection (Fig. 6A). Prior studies in our group had demonstrated that free SB202190 does not accumulate in the kidneys upon intravenous administration (Prakash et al., 2005b).

Therefore, the presence of free drug in the kidneys predominantly reflects the continuous local release of SB202190 from the conjugate within the kidneys.

Apart from serum and kidneys, we analyzed liver samples for the presence of the conjugate. Although bound drug was detectable in liver homogenates, no free drug was detected (data not shown). Furthermore, we investigated the excretion of the drug into the urine that was collected during the experimental period in metabolic cages. We observed a prolonged and continuous excretion of both free SB20190 and linker–bound drug which corresponded to the continuous release profile in the kidneys (**Fig. 7**).

Nephrotoxicity is one of the most prominent side-effects of cisplatin treatment, and is mostly associated with acute toxicity to renal tubular cells (Taguchi et al., 2005). Thus, administration of a platinum-containing compound that efficiently accumulates in the proximal tubule may induce unwanted nephrotoxicity. We therefore closely examined the animals during the pharmacokinetic study and observed no apparent discomfort up to 72h. Furthermore, we determined renal function and other parameters to determine platinum-related toxicities (Table 2). Creatinine clearance remained normal in animals receiving vehicle or conjugate while an increase in urinary protein levels was found with SB-ULS-LZM in comparison to untreated rats. However, the observed value of the conjugate-treated group was well within normal limits. Second, we detected tubular damage by TUNEL staining on kidney sections, which clearly demonstrated that cisplatin-treated animals had higher apoptotic tubular cells as compared to untreated rats. In contrast, SB-ULS-LZM-treated rats showed no increase in the number of apoptotic cells, despite the comparable levels of platinum in the kidneys of cisplatin and SB-ULS-LZM-treated groups. Morphological analysis of kidney sections using Masson staining showed no renal damage by SB-ULS-LZM treatment in comparison to control animals (Fig. 6E-G). Nephrotoxicity by cisplatin treatment was furthermore associated with a loss of body weight, while SB-ULS-

LZM treated rats showed a constant body weight during the experiment for 3 days. From these results, we concluded that the pharmacological and toxicological behavior of the linker ULS is quite different from those of the cytostatic agent cisplatin.

Effect of SB-ULS-LZM conjugate in HK-2 cells

The potential therapeutic effect of SB-ULS-LZM was evaluated in proximal tubular cell of human origin (HK-2 cells). Intracellular delivery of the conjugate is dependent on receptor-mediated endocytosis from the medium. The capability to internalize proteins is however rapidly lost in many kidney cell lines, which renders the conjugate ineffective *in vitro*, despite its efficient intratubular accumulation *in vivo*. HK-2 cells are known to internalize proteins (Gudehithlu et al., 2004) while the NRK-52E cells described earlier in this paper did not reabsorb LZM (data not shown). After incubation for 24 h with TGF-β1, we detected a 10-fold higher gene expression for procollagen–Iα1 as compared to resting levels (Fig. 8). Treatment with SB-ULS-LZM conjugate for 48 h resulted in a significant reduction by 64% of the induced gene, as did the treatment with free SB202190 (10 μM). Treatment with the LZM carrier alone did not affect the TGF-β1–induced profibrotic signaling. From these results, we concluded that the conjugate was capable to deliver pharmacologically active drug into the designated target cells.

Effect of SB-ULS-LZM conjugate in the I/R rat model

The pharmacological efficacy of SB-ULS-LZM was evaluated in the renal I/R model which finally leads to fibrosis within a period of 1-4 days. Several studies have established the involvement of activated p38 in epithelial cells after I/R injury (Furuichi et al., 2002;Mehta et al., 2002) We hypothesized that a single dose of SB-ULS-LZM would afford sufficient amounts of active drug in the kidney due to its controlled drug release profile, as

shown in Fig 6A. The conjugate was administered 2 h before ischemia so that the conjugate could accumulate completely within the kidneys. First, we examined the activation of p38 MAPkinase in the kidney by immunostaining for p-p38 positive cells. Our results confirmed that p38 was still activated after 4 days of I/R injury as compared to sham-operated animals. Vehicle—treated I/R rats had dilated and damaged tubules that strongly showed p-p38 positive cells (grade +++) in both renal cortex and medulla as compared to sham-operated animals (grade -/+). In the cortex, neither of the treatments showed any reduction in p-p38 positive cells. However, treatment with SB-ULS-LZM reduced the number of p-p38 positive cells in the medulla (grade +, Fig. 9B) but no reduction was found in SB202190—treated animals (grade +++, Fig. 9C).

Moreover, to study the effect of SB-ULS-LZM conjugate on fibrosis, we investigated the renal deposition of the fibrosis marker α -SMA by immunohistochemical analysis. We found that after 4 days of I/R injury, α -SMA expression was highly increased in the tubulointerstitial space of the renal cortex (**grade** +++, **Fig. 9D**) in comparison to shamoperated animals (**grade** -/+). A single dose of the SB-ULS-LZM conjugate reduced α -SMA expression (**grade** +++, **Fig. 9E**) whereas non-targeted SB202190 did not affect the expression of α -SMA (**grade** +++, **Fig. 9F**).

Discussion

Data from the present study confirm that blockade of p38 MAPkinase within renal tubular cells diminishes the activation of inflammatory and fibrosis related genes, which may be important for the treatment of renal fibrosis. We also demonstrated that we can deliver the p38 inhibitor SB202190 to proximal tubular cells in the kidney, and that the conjugate has a unique slow release profile. Moreover, after only a single dose of the targeted SB-ULS-LZM conjugate showed modest beneficial effects in renal ischemia-reperfusion (I/R) injured rats.

Low molecular weight proteins like LZM accumulate in the kidneys via megalinmediated endocytosis and can be exploited as renal-specific drug carriers (Haas et al., 2002). In the present study, we describe the successful coupling of SB202190 to LZM using two different linkage strategies, either employing a carbamate bond or a coordinative bond between drug and carrier. Our in vitro stability experiments demonstrated that the carbamate linkage was sensitive to serum enzymes, most likely esterases. As a consequence, free drug will be prematurely released before the SB-carbamate-LZM conjugate can reach the kidney. In contrast, the conjugate prepared with ULS displayed high stability in serum and exhibited a slow release of the drug in kidney homogenate. This slow release phenomenon can be explained by the ligand-exchange kinetics of platinum (Reedijk, 2003). Transition metals like platinum make coordination bonds with the ligands that are weaker than covalent bonds. However, the ligand-exchange behavior of platinum-coordinated compounds is quite slow, which gives them a high kinetic stability (Reedijk, 2003). GSH is a likely candidate to act as an intracellular ligand (Ikeda et al., 2001). Efficient drug displacement by GSH was proven for the present SB-ULS-LZM conjugate when it was incubated at the intracellular concentration of 5 mM GSH. In addition, the drug release might also be facilitated by cellular enzymes since kidney homogenates at pH 7.4 containing cytosolic active enzymes or at pH 5 at which lysosomal enzymes are active released SB202190 from SB-ULS-LZM. Among

others, lysosomal degradation of the LZM protein which generates methionine and cysteine residues may facilitate drug release. Other enzymes that may favor intracellular drug release are glutathione generation enzymes like thioredoxin and glutathione reductases. Based on stability and release characteristics which were favorable for SB-ULS-LZM compared to SB-carbamate-LZM, we pursued our studies with SB-ULS-LZM.

Although platinum-containing compounds such as cisplatin are considered nephrotoxic (Park et al., 2002; Wolfgang et al., 1994), ULS or SB-ULS constructs did not produce any toxicity to NRK-52E renal tubular cells even at high (100 μM) concentrations. Moreover, *in vivo* treatment with the SB-ULS-LZM conjugate did not produce any toxicity since there was no effect on renal function, renal morphology and body weight until 72 h. In addition, no increase in the number of apoptotic cells was observed, indicating the safety of SB-ULS-LZM conjugate to the kidneys.

The pharmacokinetic study indicated that SB-ULS-LZM was quickly removed from the general circulation and subsequently slowly eliminated from the renal tissue. The localization of the carrier protein in the tubular cells detected by anti-LZM staining confirms that the conjugate was reabsorbed in the tubular cells. Within these cells, the free drug was released from the conjugate almost at a constant rate during 72 h and subsequently excreted in urine. Since we found both free and linker-bound drug in the urine, it is apparent that a part of SB-ULS-LZM was not completely converted to the free drug. This suggests that the carrier protein in the conjugate was degraded by the lysosomal enzymes and released in the form of various products SB-ULS-X, in which X represents a thiol compound like methionine or any other moiety that can bind to platinum. Subsequently, SB-ULS-X released free SB202190 which was excreted in the urine and detected as a free drug, or SB-ULS-X might be eliminated by tubular cells intactly into the urine.

Our *in vitro* incubation of tubular cells with SB202190 demonstrated a reduction in the gene expressions of MCP-1, procollagen—Iα1 and TIMP-1, either induced by BSA or TGF-β1. These genes are highly relevant since they are upregulated during renal fibrosis as demonstrated by many studies (Duymelinck et al., 2000; Grygielko et al., 2005; Lloyd et al., 1997). The effect of SB202190 on albumin—induced fibrotic markers was less strong than at TGF-β1 induced genes. This may be explained by the nature of albumin-induced gene expression in tubular cells, which causes the activation of several other signaling pathways apart from p38 MAPkinase (Burton et al., 1999; Yard et al., 2001). We examined the activity of the SB-ULS-LZM conjugate in HK-2 cells which are known for their capacity to internalize proteins via endocytosis (Gudehithlu et al., 2004). Incubation of the HK-2 cells with TGF-β1 activated profibrotic signaling, which was substantially (64 %) reduced by preincubation with the SB-ULS-LZM conjugate. Since our *in vitro* stability studies had demonstrated that less than 10 % of the coupled drug was released in the cell culture medium, such an effect can only be effectuated after internalization and processing of the conjugate into active drug.

We examined the efficacy of SB-ULS-LZM after renal I/R injury since p38 is activated in renal tubular cells after ischemia (Furuichi et al., 2002; Mehta et al., 2002) and I/R injury finally leads to fibrosis (Jain et al., 2000). Our data on p-p38 staining confirmed that p38 is still activated in tubular cells 4 days after I/R injury and p-p38 positive cells were well-correlated with the injured tubules. Furthermore, we demonstrated that a single dose of SB-ULS-LZM was capable of lowering p38 activation, which is in line with the continuous levels of free drug. A reduction in p-p38 positive cells was only found in the renal medulla but not in the cortex, which is the primary site of proximal tubular cells. Either SB202190, released from the conjugate, redistributed from the cortical tubular cells to the medulla and exerted the effect over there or the effect in the cortex was not visualized due to the very high

activation of p38 in the cortex. Most likely, the latter is the case because the expression of the fibrosis marker α -SMA in the cortex was reduced. In contrast to SB-ULS-LZM, non-delivered SB202190 did not affect the expression of either p-p38 or α -SMA, presumably since the free drug is rapidly eliminated from the body and does not reach the kidney in high levels during the four-day period. Since we have administered similar amounts of SB202190 in either treatment group, we can attribute the improved efficacy of SB202190 to its renal delivery. Further studies are however needed to elucidate the mechanism of action of the conjugate, and how p38 activation in different cell types is involved.

We conclude that p38 MAPkinase inhibition in proximal tubular cells is in potential an interesting approach to treat renal fibrosis. Such a strategy involves the development of a renal specific conjugate that can successfully deliver p38 MAPkinase inhibitors to the renal tubular in the kidney. Our new linkage technology ULS produced drug-LZM conjugates that display a sustained release of the drug in tubular cells for several days, which is an advantageous characteristic for drugs against chronic diseases. In addition, a large number of drugs containing nitro-aromatic rings such as pyridine, pyrimidine or imidazole groups (Laufer and Wagner, 2002; English and Cobb, 2002), may be potential candidates for the ULS coupling approach.

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Footnotes

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Reprint requests

Jai Prakash

Department of Pharmacokinetics and Drug Delivery

Groningen University Institute for Drug Exploration

Antonius Deusinglaan 1

9713 AV, Groningen

The Netherlands

Email: j.prakash@rug.nl

Tel: +31-50-3633281

Fax: +31-50-3633247

Legends for Figures

Figure 1. Effects of SB202190 on albumin or TGF-β1 induced gene expressions of MCP-1 (**A**), procollagen-Iα1 (**B**) and TIMP-1 (**C**) in NRK-52E cells. Cells were grown to 80% confluency in 12-well plates and then deprived from serum for 24 h. Thereafter the cells were preincubated for 2 h with SB202190 (10 μM) and then activated with either BSA (30 mg/ml) or TGF-β1 (10 ng/ml) for 24 h. After that, cells were harvested for RNA isolation. The mRNA expressions were determined by quantitative RT-PCR. Data represent the mean \pm SEM for at least 3 independent experiments. Differences versus control are presented as $^{\dagger}p$ <0.05, $^{\dagger\dagger}p$ <0.01 and $^{\dagger\dagger\dagger}p$ <0.001. Other differences are $^{\ast}p$ <0.05, $^{\ast\ast}p$ <0.01, $^{\ast\ast\ast}p$ <0.001.

Figure 2. Synthesis scheme of SB-carbamate-LZM (**A**) and SB-ULS-LZM conjugates (**B**). Large filled circles represent LZM. NSED, N-succinimidyl-N-boc-ethylenediamine; TFA, trifluoroacetic acid; GMBS, γ-maleimidobutyryloxysuccinimide ester; SATA, N-Succinimidyl-S-acetylthioacetate; ULS, Universal Linkage System.

Figure 3. Release of SB202190 from SB-carbamate-LZM (**A**) and SB-ULS-LZM (**B**) in different conditions. The experiment was performed in triplicate, mean \pm SEM.

Figure 4. Comparison of cellular toxicity of different platinum containing compounds on renal tubular cells (NRK-52E). Cells were incubated for 24h with indicated compounds, after which cell viability was determined by the Alamar blue assay. Concentrations tested corresponded to 10 and 100 μ M platinum, or were equivalent to the amount of drug (SB202190) or protein (LZM). Data represent the mean \pm SEM for 3 independent experiments. **p<0.01.

Figure 5. Serum disappearance curve of SB-ULS-LZM. Symbols represent the % dose of SB202190 at each time point; the continuous line represents the pharmacokinetic data-fit curve (two-compartment model).

Figure 6. Renal levels of SB-ULS-LZM (A). Symbols represent the % dose of SB202190 at each time point and the continuous line represents the pharmacokinetic data-fit curve. The curve-fitting was performed with Multi-fit software by two-compartment model including peripheral drug levels. Anti-LZM immunohistochemical staining (B-D) on kidney sections. Untreated animals (B); SB-ULS-LZM treated animals at 1 h (C, D). Arrows in C and D indicate the staining for lysozyme in tubular cells. Panel C (magnification 200×) shows accumulation of SB-ULS-LZM in kidneys, which appeared to be allocated within the tubular cells as observed at magnification 400× (D). Masson staining shows renal morphology in untreated animals (E) and SB-ULS-LZM treated animals at 24 h (F) and 72 h (G), at 200× magnification. There is no change in the morphology of the proximal tubular cells after 24 h (E vs. F) or 72 h (E vs. G) after administration of the conjugate.

Figure 7. Urinary excretion rate of free and linker–bound SB202190 after administering the conjugate. Symbols represent the % dose/ 24h of SB202190 at each time point and the continuous line represents the fitted curve.

Figure 8. Effects of SB202190 and SB-ULS-LZM on the gene expressions of procollagen-Iα1 induced by TGF-β1 in HK-2 cells. Cells were grown to the 80% confluency and then deprived from serum for 24 h. The SB-ULS-LZM conjugate (SB-ULS-LZM, 155 μg/ml) or methionine-modified LZM (LZM, 155 μg/ml) were incubated at the time of serum

deprivation whereas SB202190 (10 μ M) was added 1 h before adding TGF- β 1 (10 ng/ml) to the cells. The cells were further cultured for 24 h. Then cells were harvested for RNA isolation. The mRNA expressions were determined by quantitative RT-PCR. Data represent the mean \pm SEM for at least 3 experiments. Differences versus control is presented as $^{\dagger\dagger\dagger}p<0.001$. Other differences are **p<0.01.

Figure 9. Representative photomicrographs of the immunohistochemical detection of p-p38 positive cells in renal medulla (**A-C**; **200**×) and α-SMA expression in renal cortex (**D-F**; **100**×), 4 days after unilateral ischemia–reperfusion injury. Vehicle–treated animals (**A, D**); SB-ULS-LZM–treated animals (**B, E**); SB202190–treated animals (**C, F**). Arrows in panels **A-C** indicate the immunolocalization (dark brown color) of p-p38 positive nuclei in the tubular cells corresponding to the dilated and injured tubules. Arrows in panels **D-F** indicate the localization of α-SMA in tubulointerstitial space with red color.

Table 1 Pharmacokinetic parameters (two-compartment model) derived from serum concentration-time curves after a single intravenous dose of 16 mg/kg (equivalent to 376 μg/kg SB202190) of SB-ULS-LZM in rats.

Parameters	units	Values	
	umts	$(mean \pm SE)$	
V1	ml/kg	101 ± 18	
$\mathrm{CL}_{\mathrm{ini}}$	ml/kg/h	149 ± 28	
CL	ml/kg/h	24.0 ± 1.5	
$\mathrm{AUC}_{(0\text{-}\infty)}$	h.µg/ml	15.6 ± 1.0	
$t_{1/2}\alpha$	h	0.41 ± 0.1	
$t_{1/2}\beta$	h	18.7 ± 1.8	

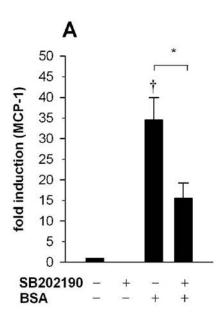
V1, volume of central compartment; CL_{ini} , sum of elimination and distribution clearance from central compartment; CL, Total serum clearance; $AUC_{(0-\infty)}$, area under the curve from zero to infinity; $t_{1/2} \alpha$, distribution half life; $t_{1/2} \beta$, elimination half life

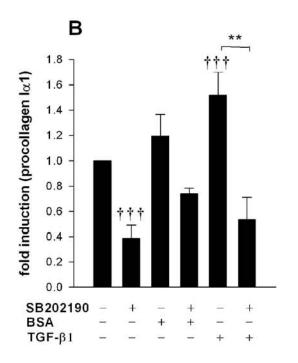
Table 2. Summary of the parameters to determine platinum–related nephrotoxicity in SB-ULS-LZM and cisplatin –treated animals.

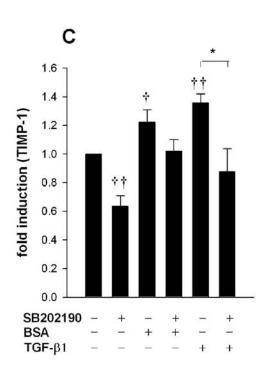
Parameters	Untreated group	SB-ULS-LZM -treated group	Cisplatin-treated group
Creatinine clearance (ml/min)	1.0 ± 0.13	0.8 ± 0.03	1.1 ± 0.13
Urinary protein levels (mg/d)	19.16 ± 1.3	$29.6 \pm 2.0^{\dagger\dagger}$	23 ± 3.6
TUNEL positive cells (numbers per field)	46.4 ± 4.14	42.7 ± 18**	$187 \pm 26^{\dagger\dagger}$
Renal platinum concentration (nmol/g)	N.D.	37.0 ± 1.2**	28.4 ± 0.8
Change in body weight (%)	-1.75 ± 2.25	+0.3 ± 1.2*	$\text{-}5.0 \pm 0.6^{\dagger\dagger}$

Data for untreated and cisplatin groups are represented as mean \pm SEM, n=4 at 24 h. The values for SB-ULS-LZM are shown as mean \pm SEM, n=4 at 24, 32, 48 and 72 h except for TUNEL positive cells which is n=5 at 24 (n=2), 32, 48 and 72 h. The differences between cisplatin and SB-ULS-LZM groups are *p<0.05, **p<0.01. The differences versus untreated groups are p<0.05, *p<0.01. N.D., not detectable.

Figure 1

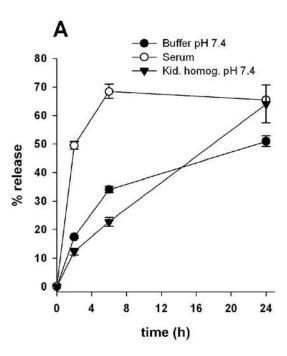


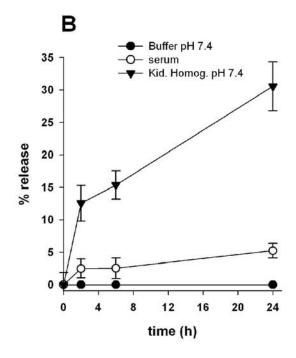


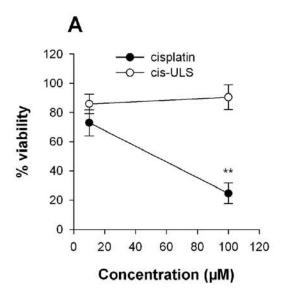


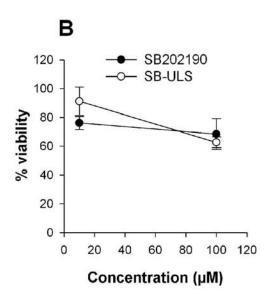
SB-ULS-lysozyme

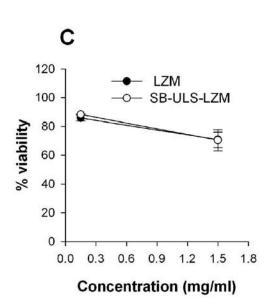
NH-BOC

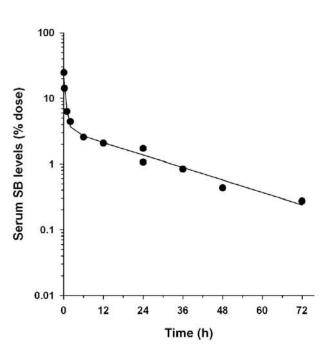


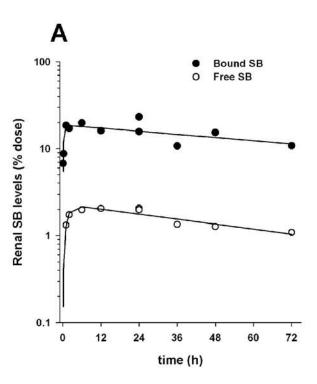


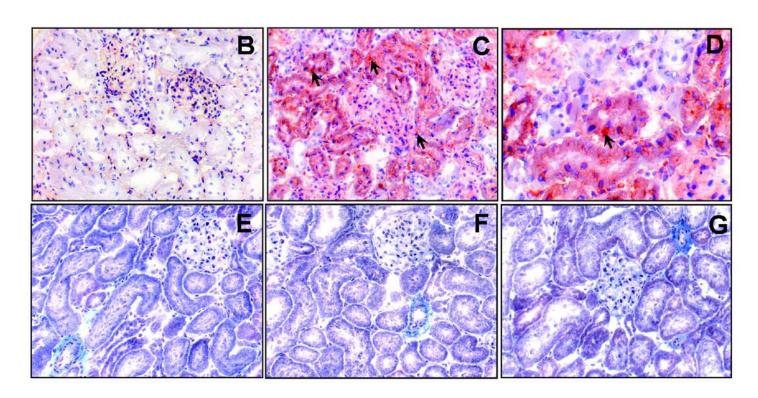


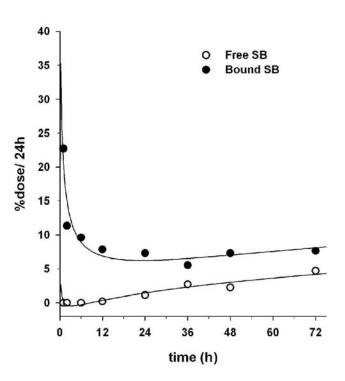












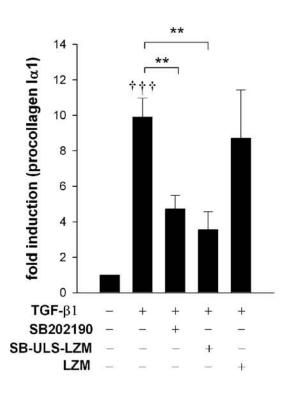


Figure 9

